

Predicting Emergent Behavior in Cardiac Tissue: A Grand Challenge

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SUNY at Stony Brook**

Joint work with

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James Glimm, Colas Le Guernic, and Scott A. Smolka**

Excitable Cells

- Generate action potentials (elec. pulses) in response to electrical stimulation
 - Examples: neurons, cardiac cells, etc.
- Local regeneration allows electric signal propagation without damping
- Building block for electrical signaling in brain, heart, and muscles

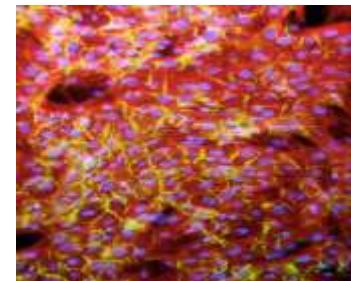


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Neurons of a squirrel
University College London



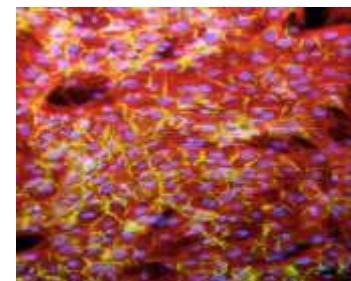
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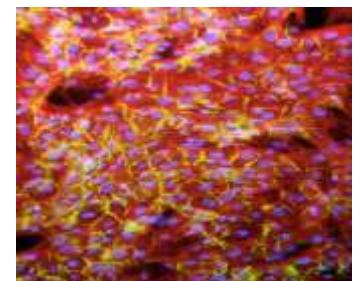
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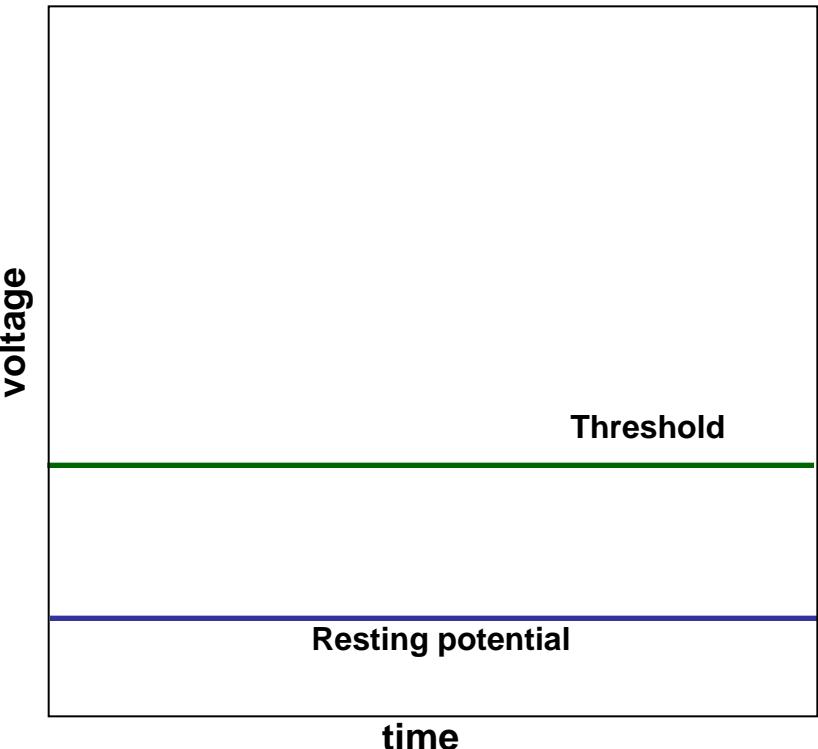
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Single Cell Reaction: Action Potential

Membrane's AP depends on:

- Stimulus (voltage or current):
 - External / Neighboring cells
- Cell itself (excitable or not):
 - State / Parameters value

Schematic Action Potential

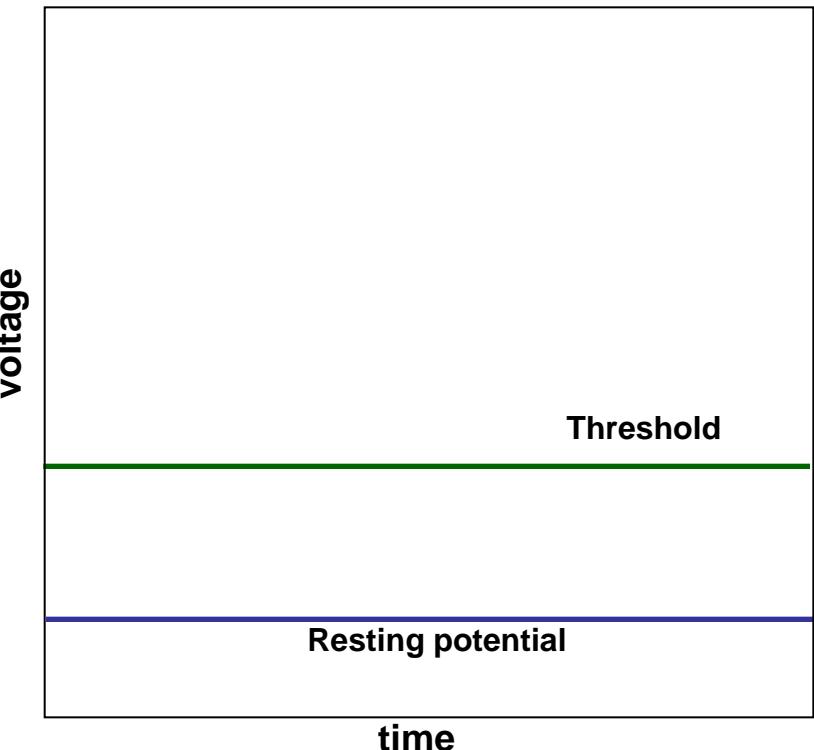


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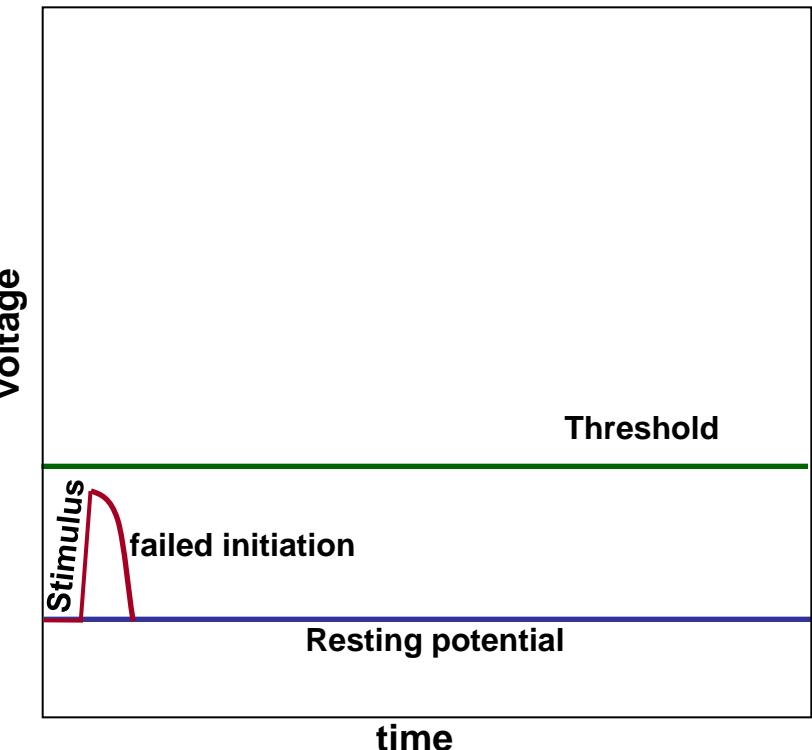


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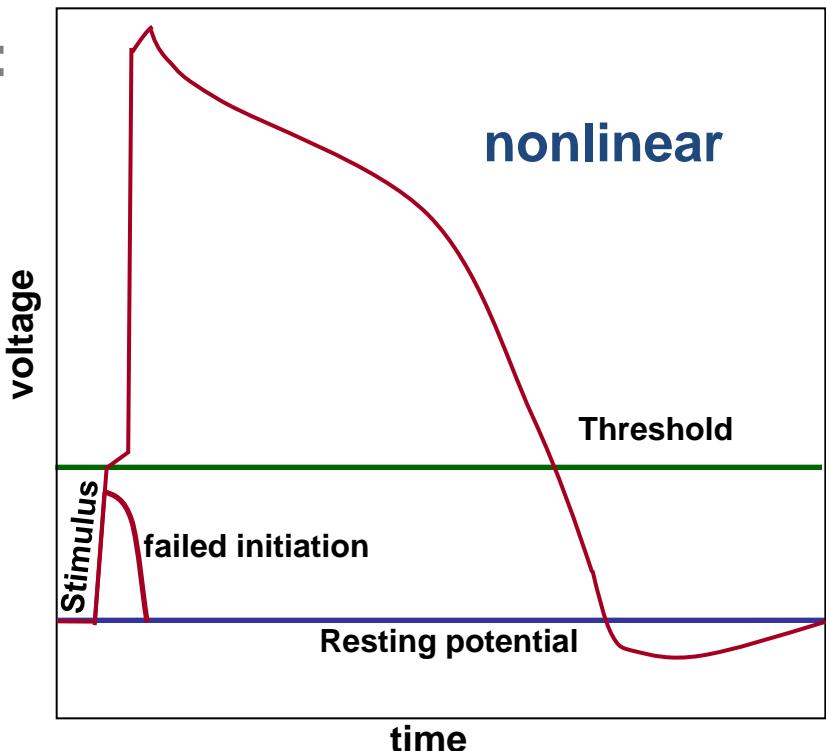


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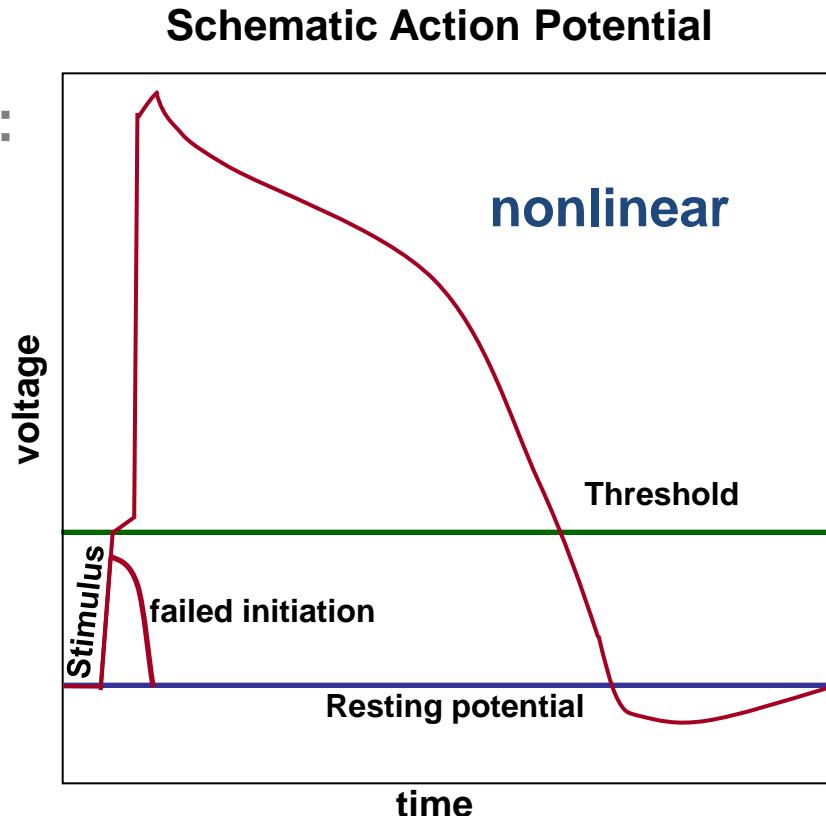
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$$\frac{\partial \mathbf{u}}{\partial t} = R(\mathbf{u}) + \nabla(D\nabla\mathbf{u})$$



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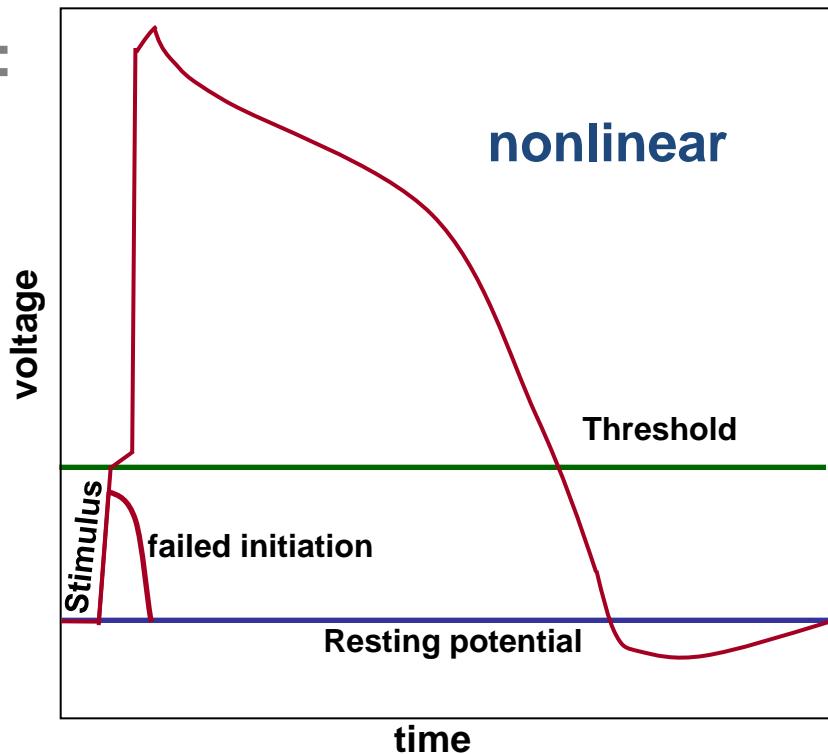
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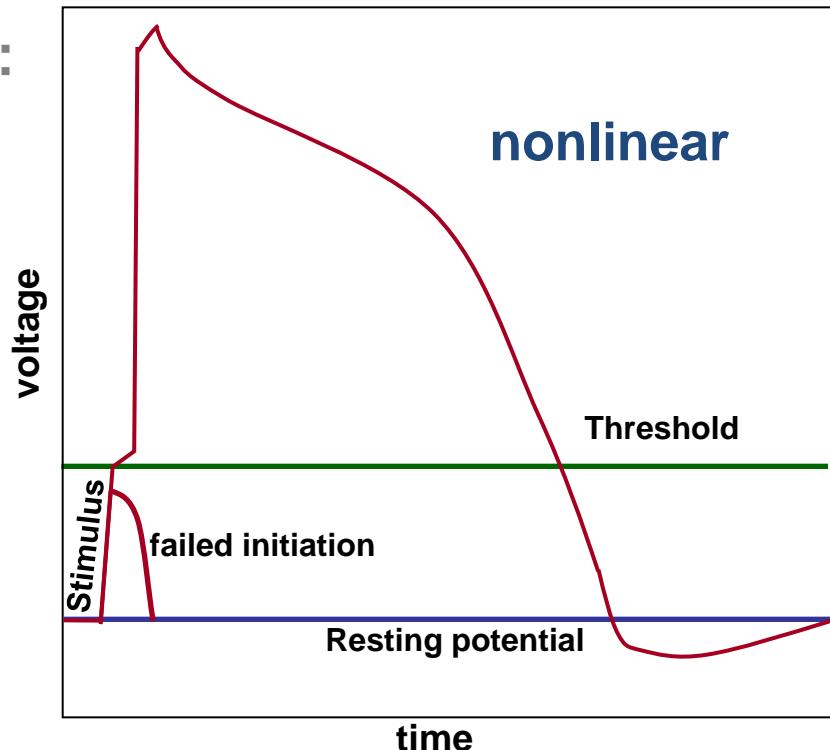
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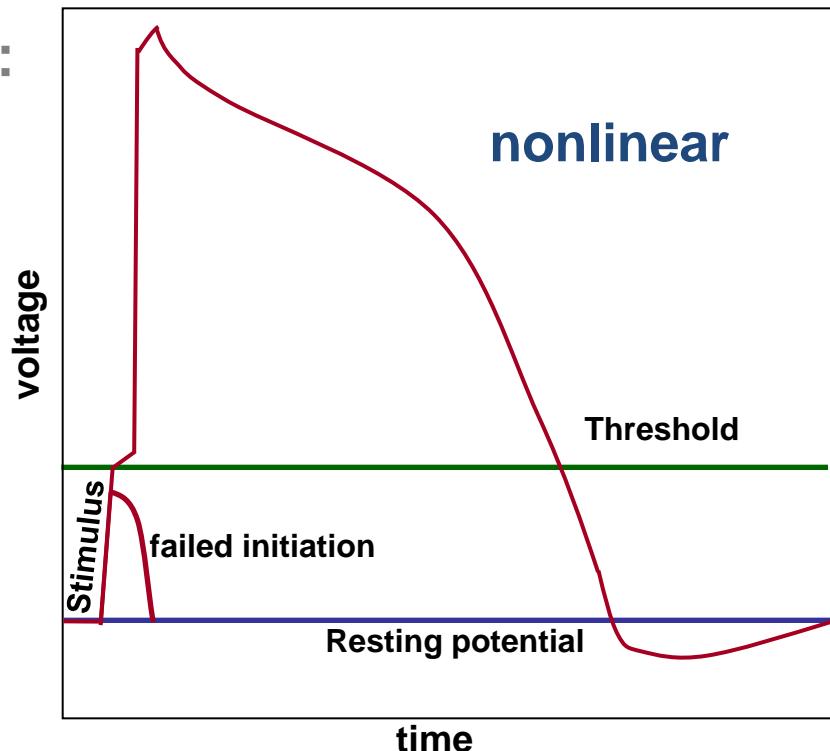
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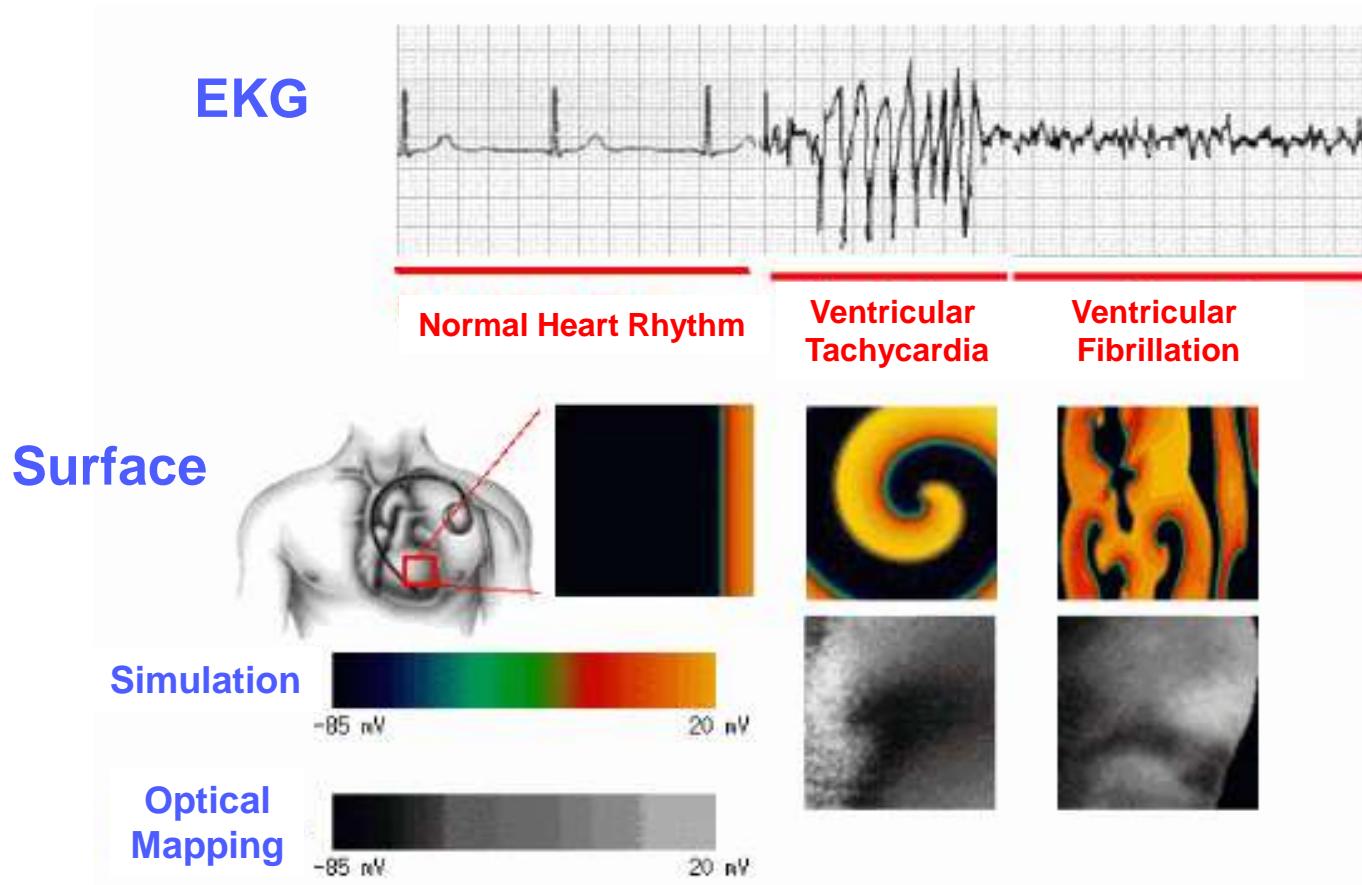
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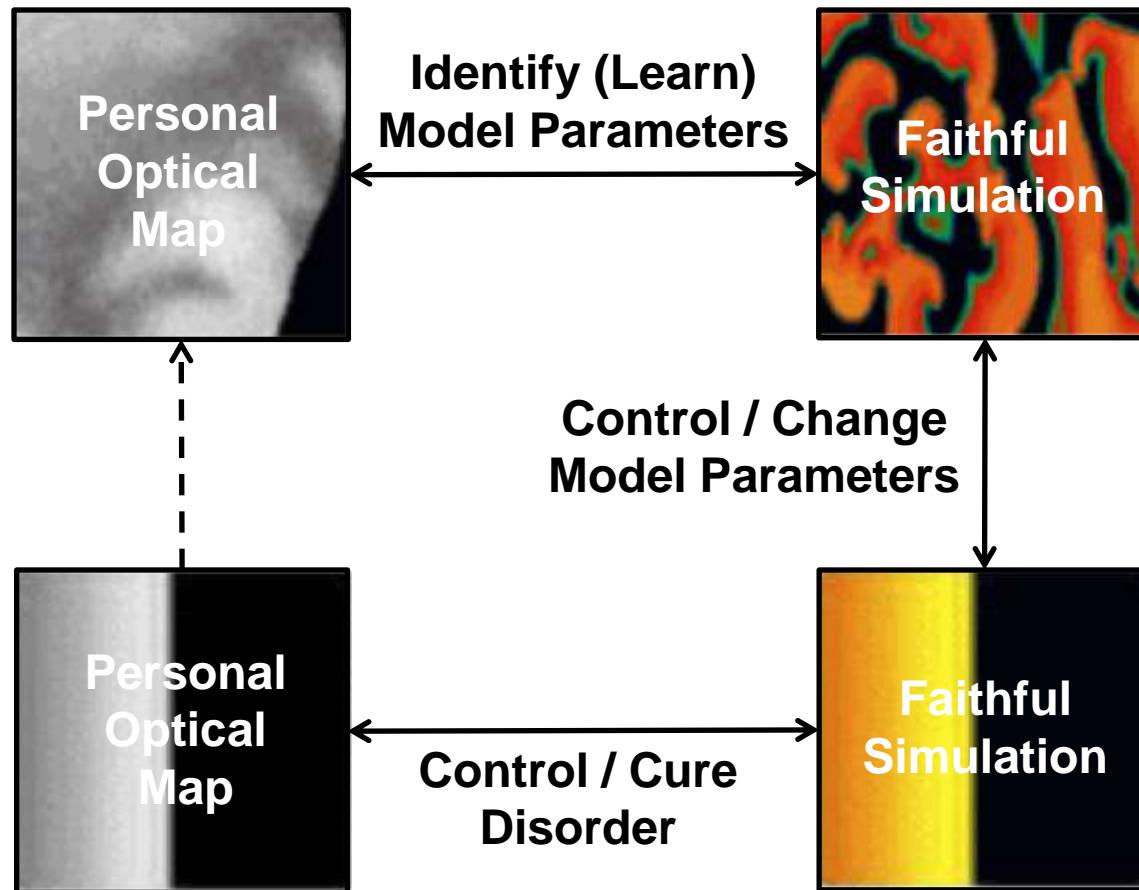


Emergent Behavior in Cardiac Cells



Arrhythmia afflicts more than 3 million Americans alone

The Grand SB-Challenge



Human Cardiac-Cell Models

Iyer-Mazhari-Winslow-04

Variables: 67

Parameters: 94

Most Detailed Ionic Model

- Latest experimental data
- Multi-affine ODE (MA law)

Human Cardiac-Cell Models

Tusscher-Noble²-Panfilov-03

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Parameters: 44

Less Detailed Ionic Model

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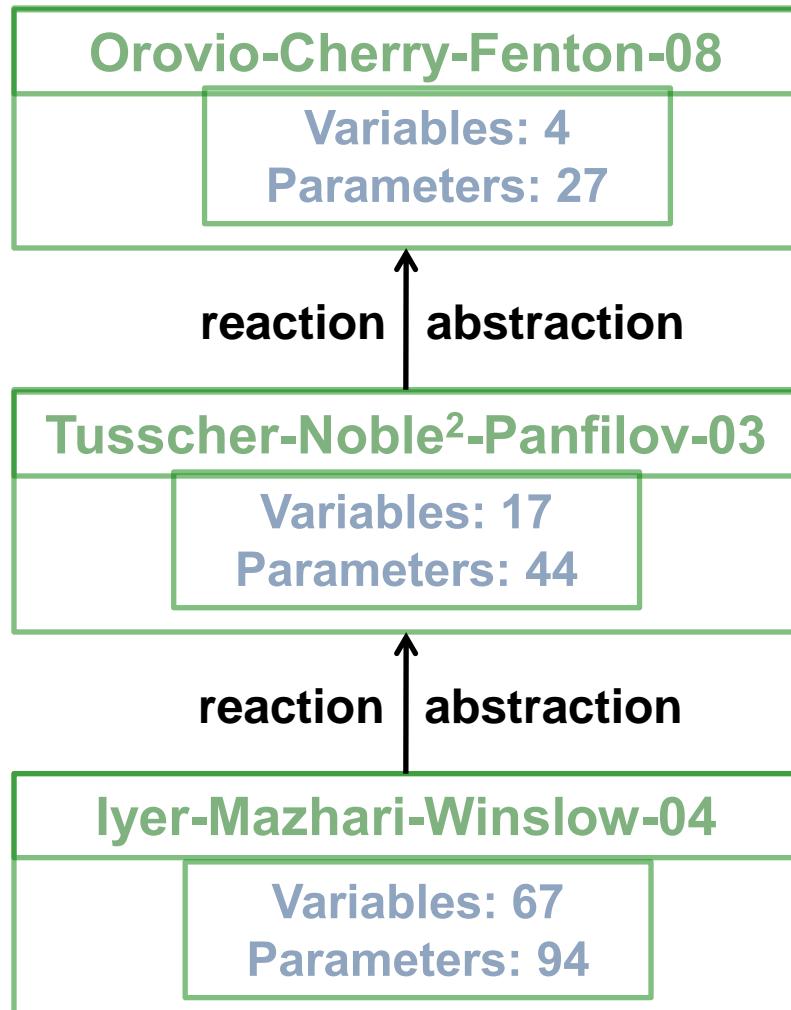
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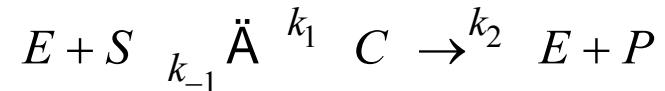
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Enzymatic Reactions (QSSA)



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$$d[C] / dt = k_1[E][S] - (k_{-1} + k_2)[C]$$

$$d[P] / dt = k_2[C]$$

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Assume $E = S$ and express E :

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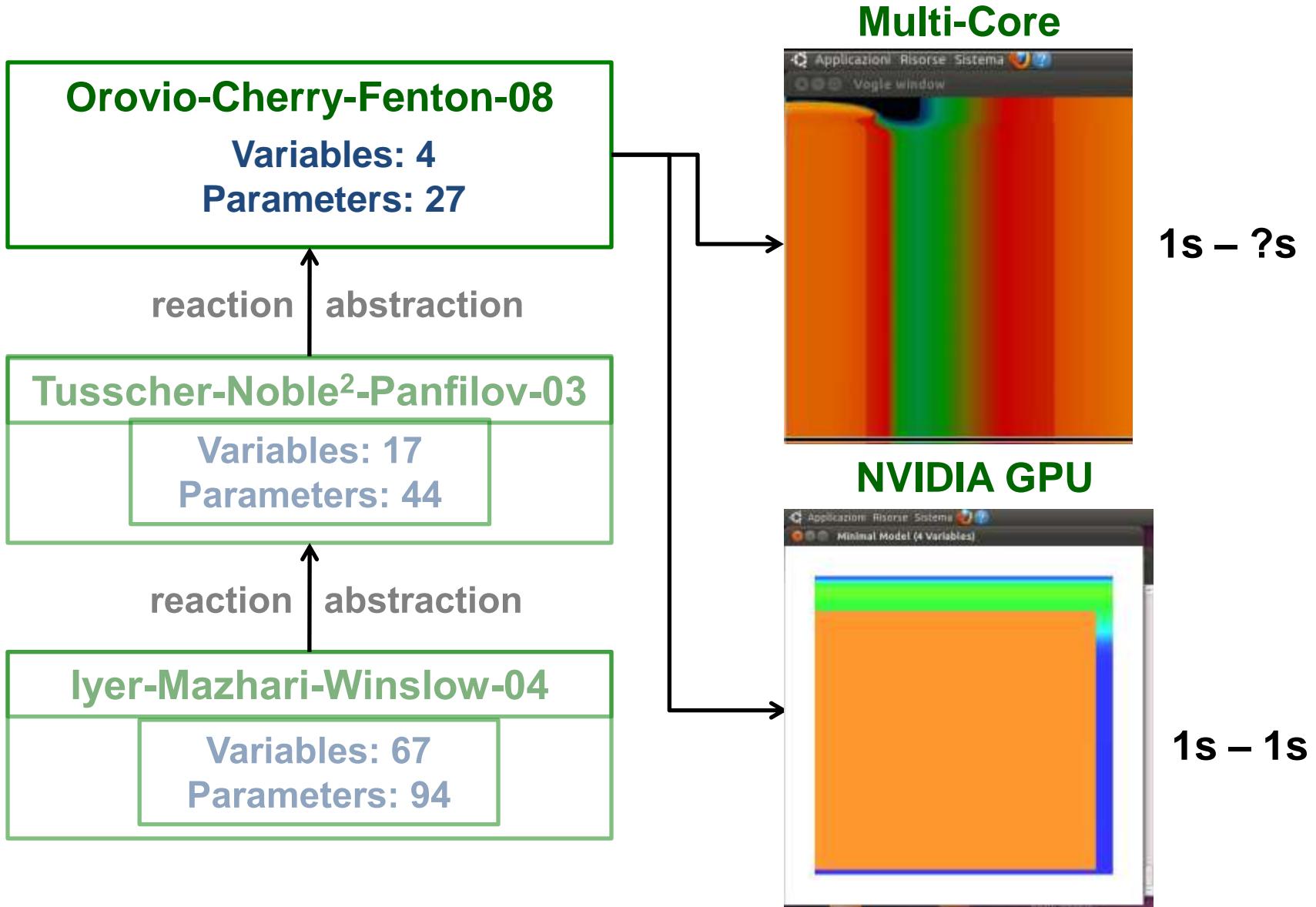
$$[E] = [E_t] - [C]$$

Michaelis-Menten Relation (Sigmoidal):

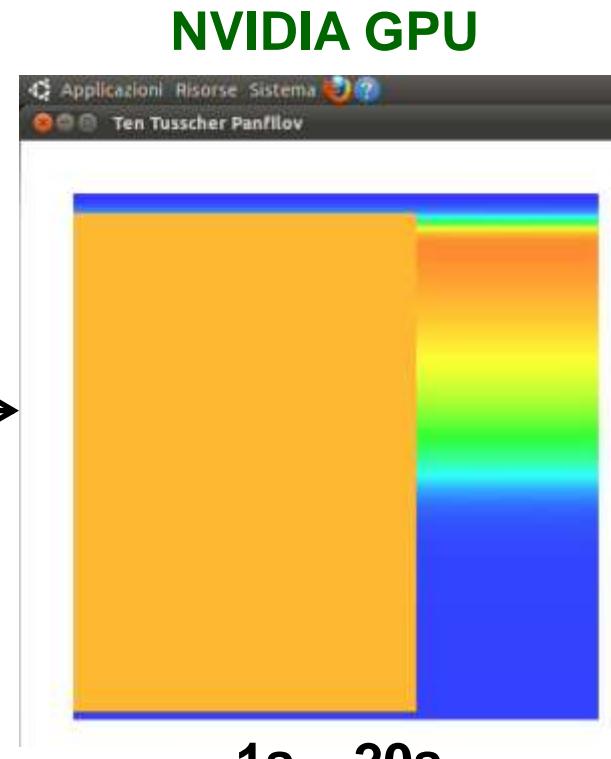
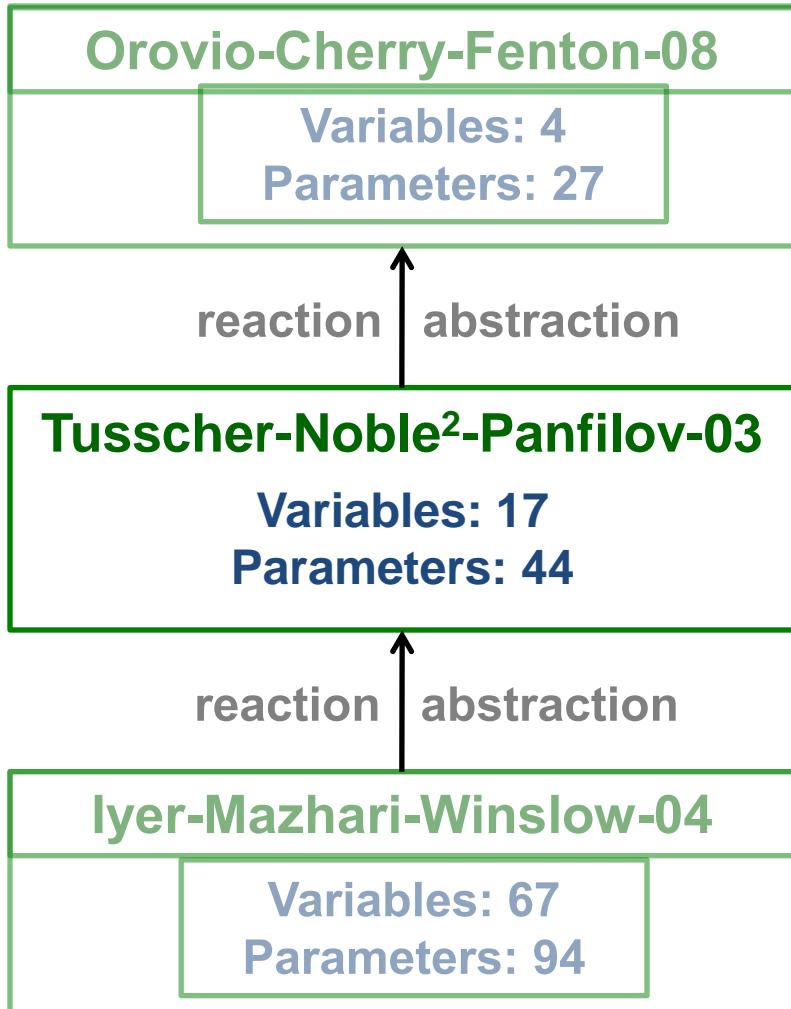
$$d[P] / dt = a / (1 + e^{-(u-\theta)}) = a \mathbf{S}^+(u, \theta, 1)$$

$$u = \ln[S], \quad a = k_2 E_t, \quad \theta = \ln(k_{-1} + k_2) / k_1$$

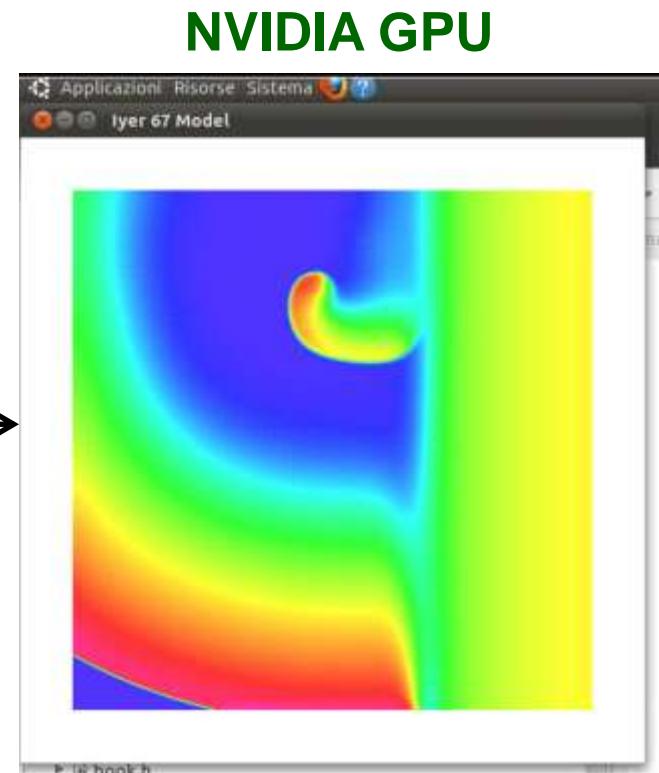
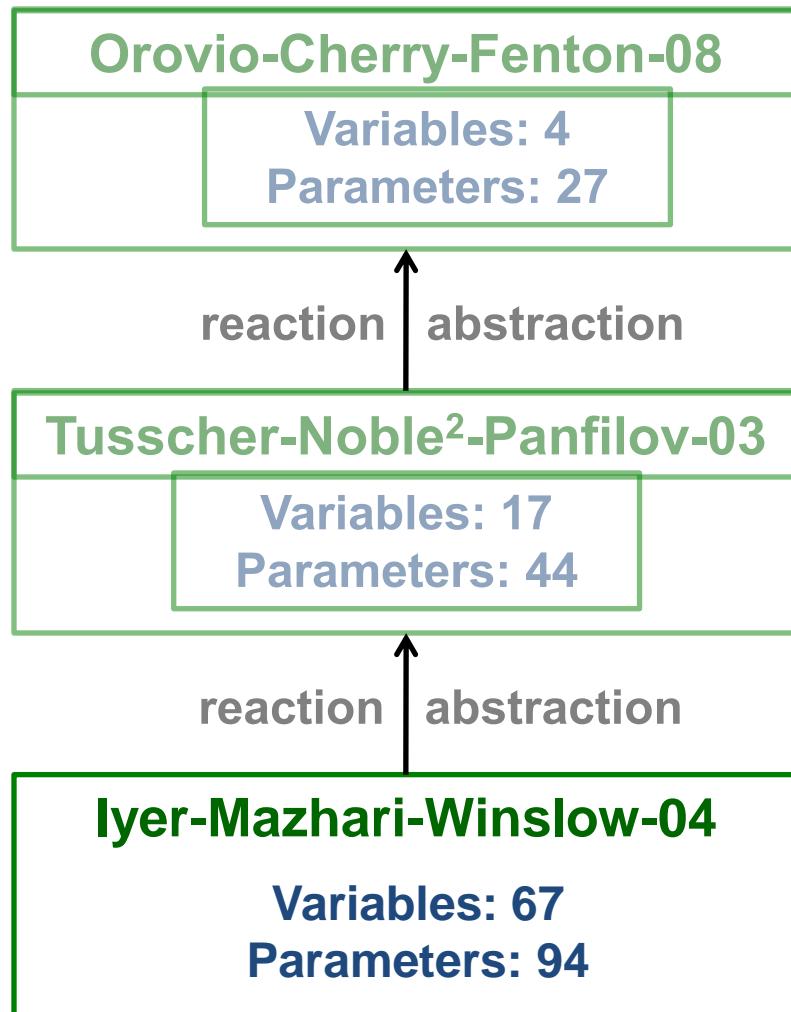
Simulation: Hardware and Dimension



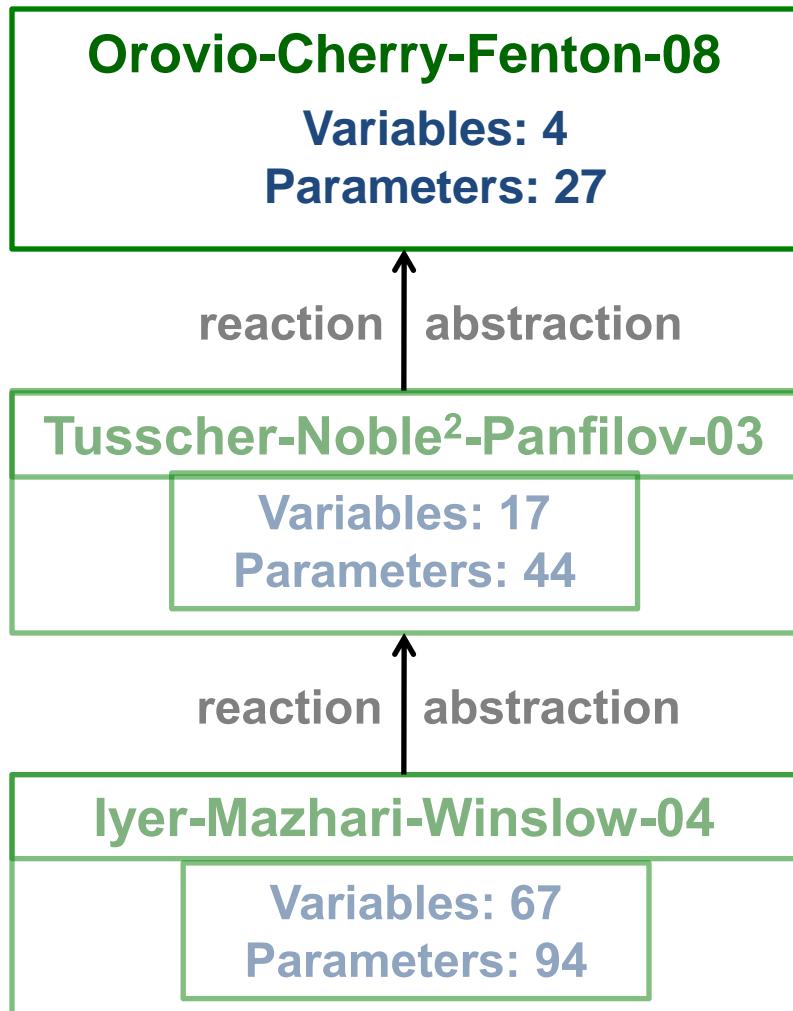
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Param. Estim: Hardware and Dimension



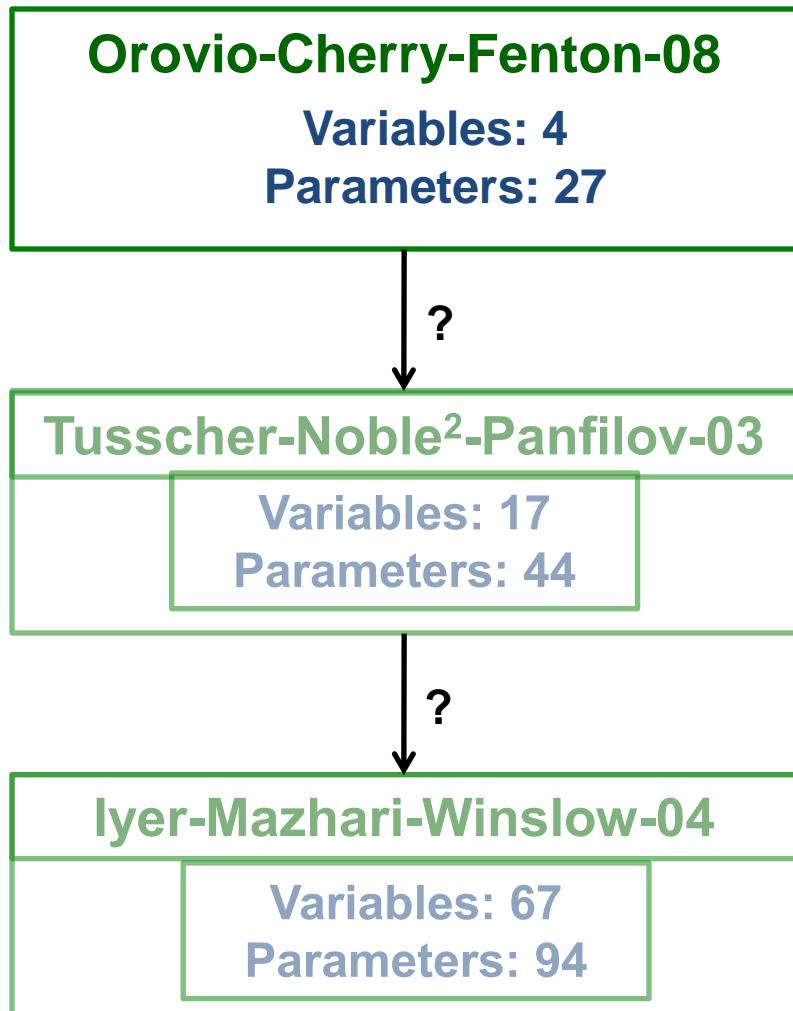
Hardware matters:

- Implem. SpaceEx in CUDA
- Extend SpaceEx to MA ODE

Dimension matters:

- Work on OCF model (MRM)
- MRM still intractable
- Will talk about our approach

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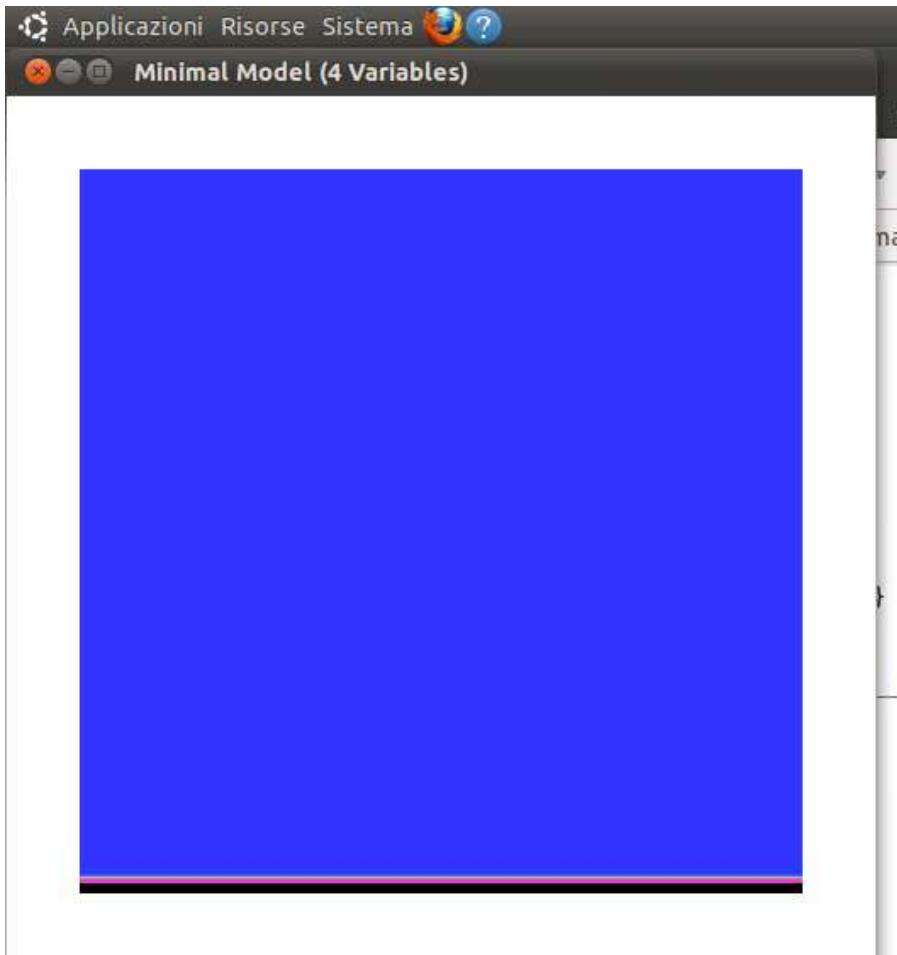
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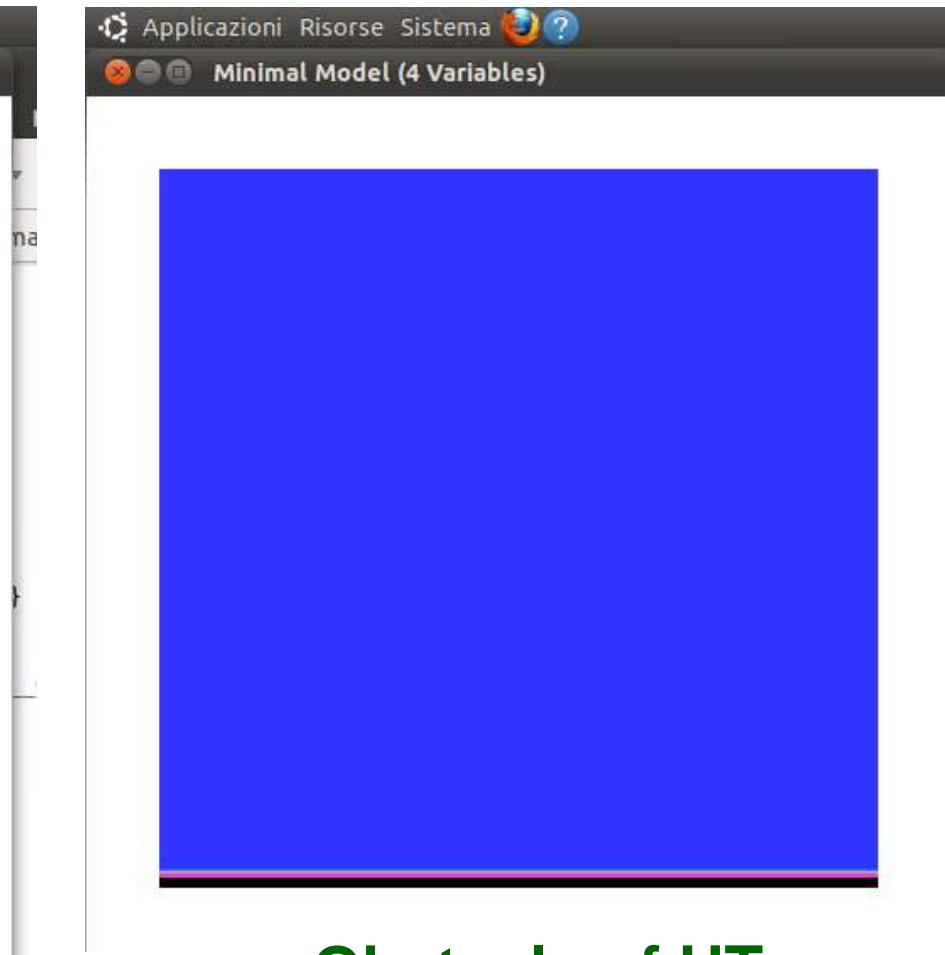
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Lack of Excitability: Implications

Stimulus: bottom row, every 300ms



No Obstacle



Obstacle of UT

Problem to Solve

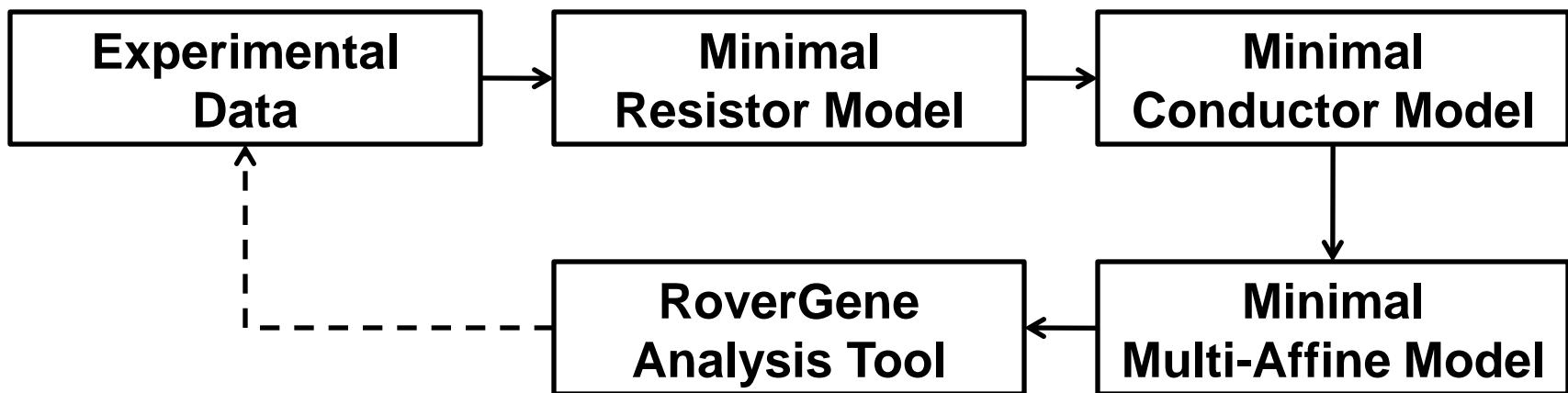
- What circumstances lead to a loss of excitability?
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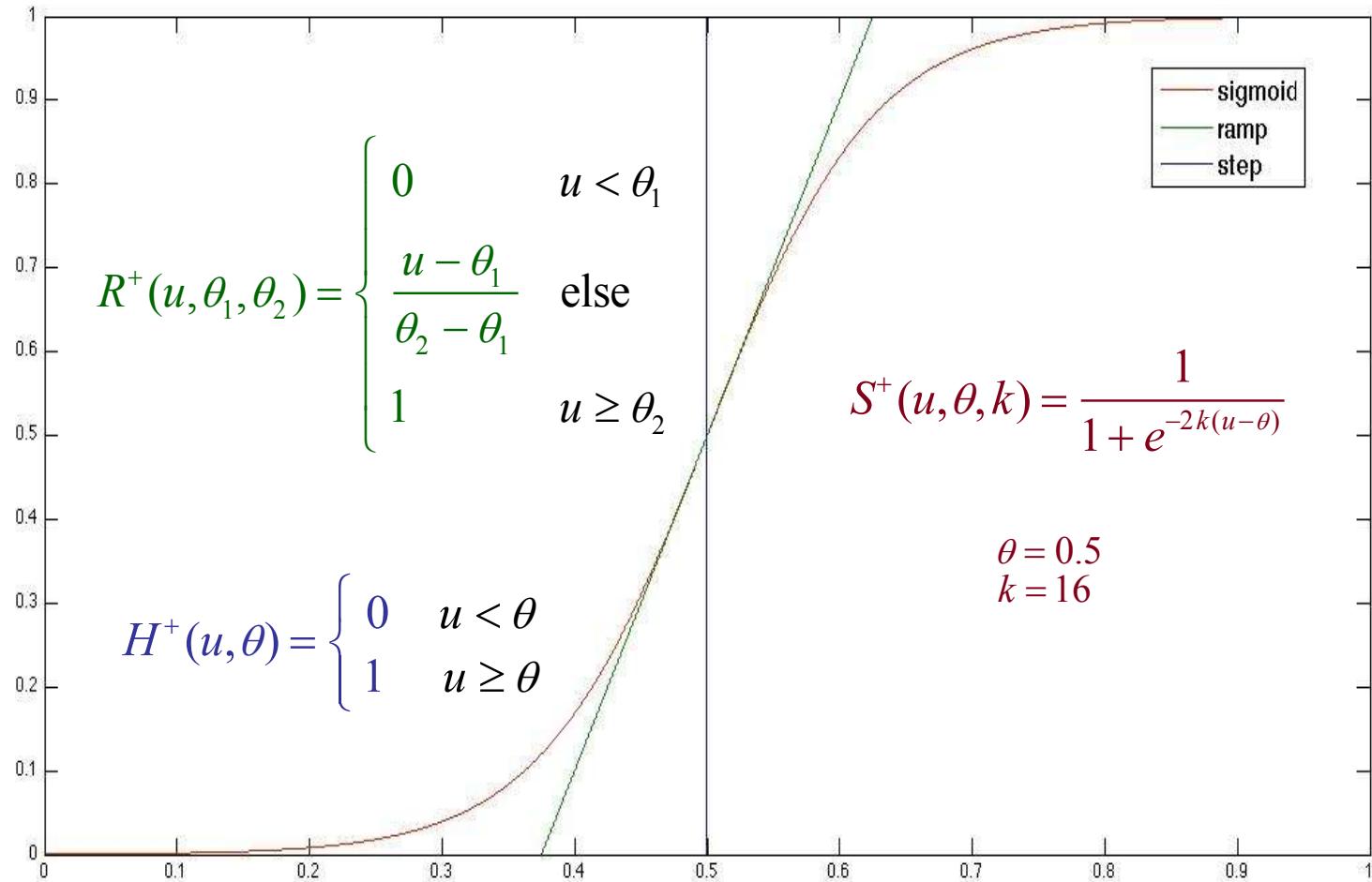
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Biological Switching

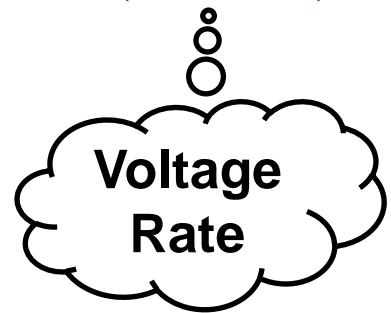


Minimal Resistor Model: Voltage ODE

$$\dot{u}(u, v, w, s) = \nabla(D\nabla u) - (J_{fi}(u, v) + J_{si}(u, w, s) + J_{so}(u))$$

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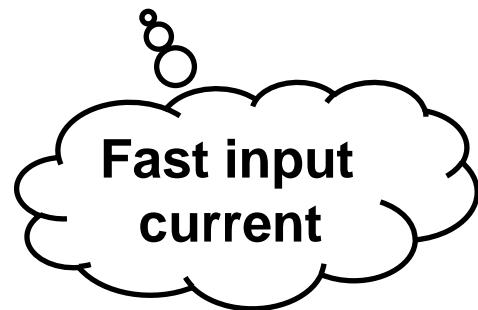
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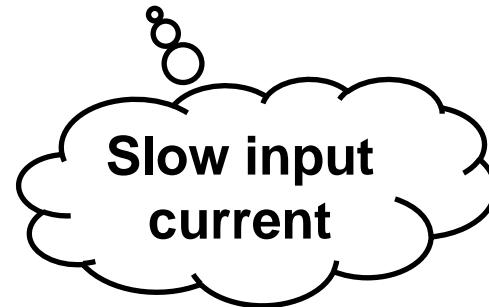
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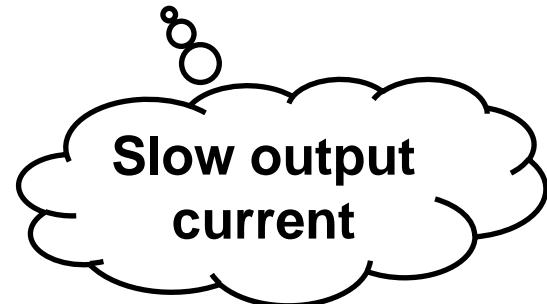
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MRM: Currents Equations

$$\dot{u}(u, v, w, s) = \nabla(D\nabla u) - (J_{fi}(u, v) + J_{si}(u, w, s) + J_{so}(u))$$

$$J_{fi}(u, v) = -H^+(u, \theta_v) (\textcolor{red}{u} - \theta_v)(u_u - \textcolor{red}{u})\textcolor{red}{v} / \tau_{fi}$$

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∞

Piecewise
Nonlinear

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Piecewise
Bilinear

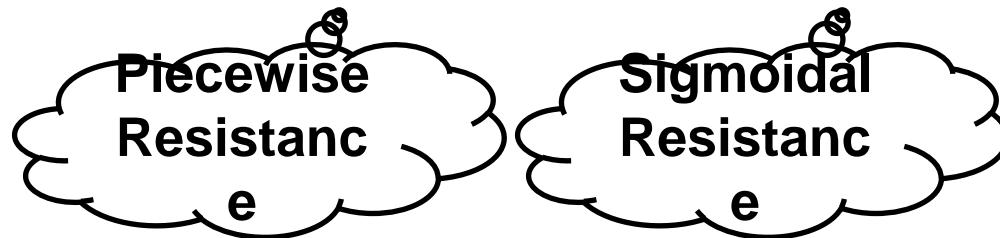
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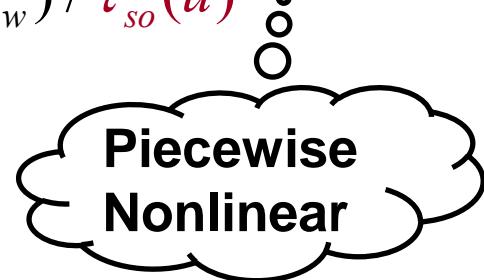
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$$\dot{w}(u, w) = H^-(u, \theta_w) (w_\infty - w) / \tau_w^-(u) - H^+(u, \theta_w) w / \tau_w^+$$

$$\dot{s}(u, s) = (S^+(u, u_s, k_s) - s) / \tau_s(u)$$



MRM: Voltage-Controlled Resistances/SSV

$$\tau_v^-(u) = H^-(u, \theta_o) \tau_{v_1}^- + H^+(u, \theta_o) \tau_{v_2}^-$$

$$\tau_s(u) = H^-(u, \theta_w) \tau_{s_1} + H^+(u, \theta_w) \tau_{s_2}$$

$$\tau_o(u) = H^-(u, \theta_o) \tau_{o_1} + H^+(u, \theta_o) \tau_{o_2}$$



MRM: Voltage-Controlled Resistances/SSV

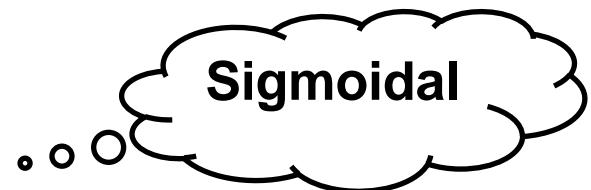
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$$\tau_w^-(u) = \tau_{w_1}^- + (\tau_{w_2}^- - \tau_{w_1}^-) S^+(u, u_s, k_w^-)$$

$$\tau_{so}(u) = \tau_{so_1} + (\tau_{so_2} - \tau_{so_1}) S^+(u, u_s, k_{so})$$



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$$\tau_{so}(u) = \tau_{so_1} + (\tau_{so_2} - \tau_{so_1})$$

Piecewise
e
Constant

$$v_\infty(u) = H^-(u, \theta_o)$$



$$w_\infty(u) = H^-(u, \theta_o) (1 - u / \tau_{w\infty}) + H^+(u, \theta_o) w_\infty^*$$



MRM: Scaled Steps and Sigmoids

$$\tau_v^-(u) = H^+(u, \theta_o, \tau_{v_1}^-, \tau_{v_2}^-)$$

$$\tau_s(u) = H^+(u, \theta_w, \tau_{s_1}, \tau_{s_2})$$

$$\tau_o(u) = H^+(u, \theta_o, \tau_{o_1}, \tau_{o_2})$$



MRM: Scaled Steps and Sigmoids

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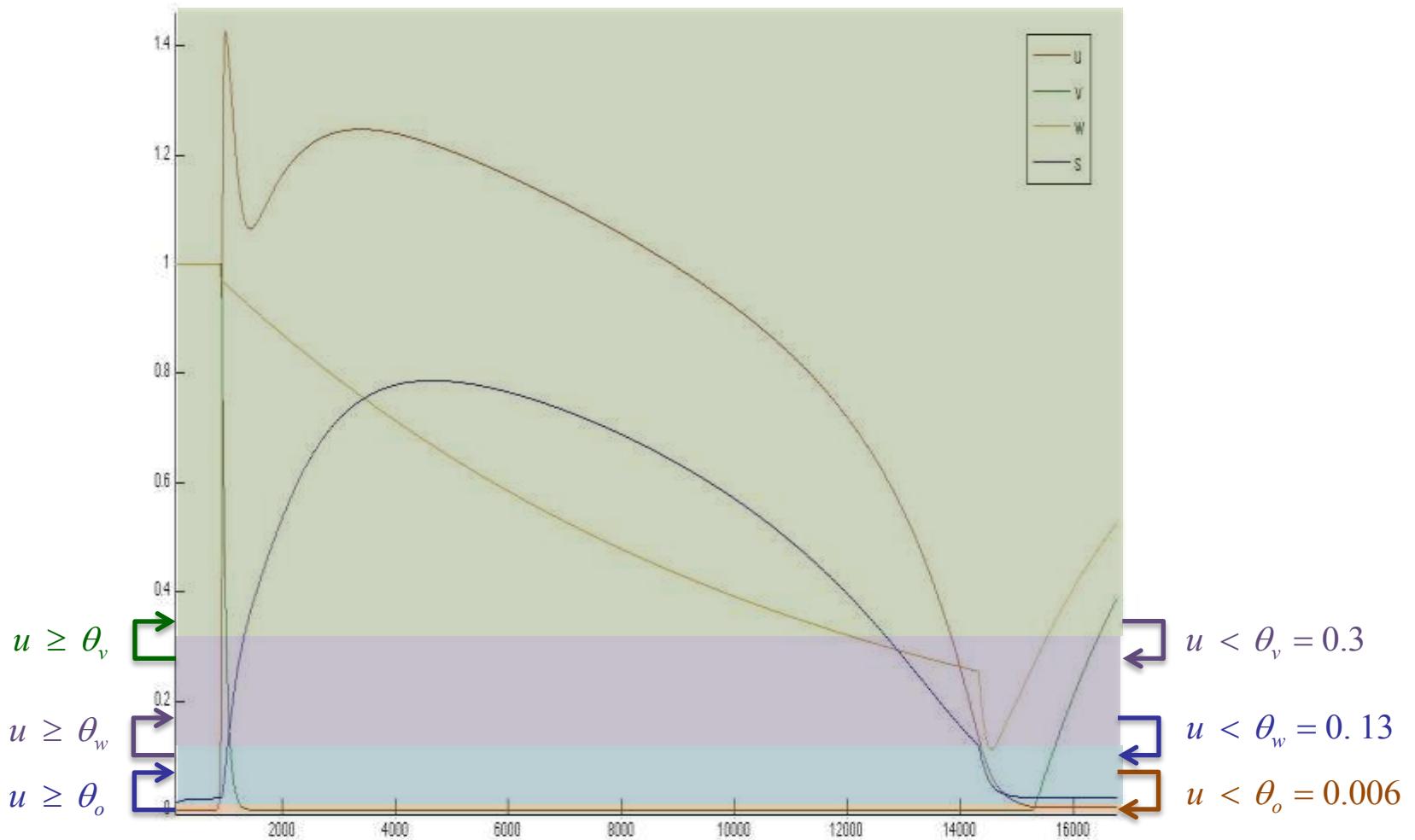
$$\tau_o(u) = H^+(u, \theta_o, \tau_{o_1}, \tau_{o_2})$$

$$\tau_w^-(u) = S^+(u, u_s, k_w^-, \tau_{w_1}^-, \tau_{w_2}^-)$$

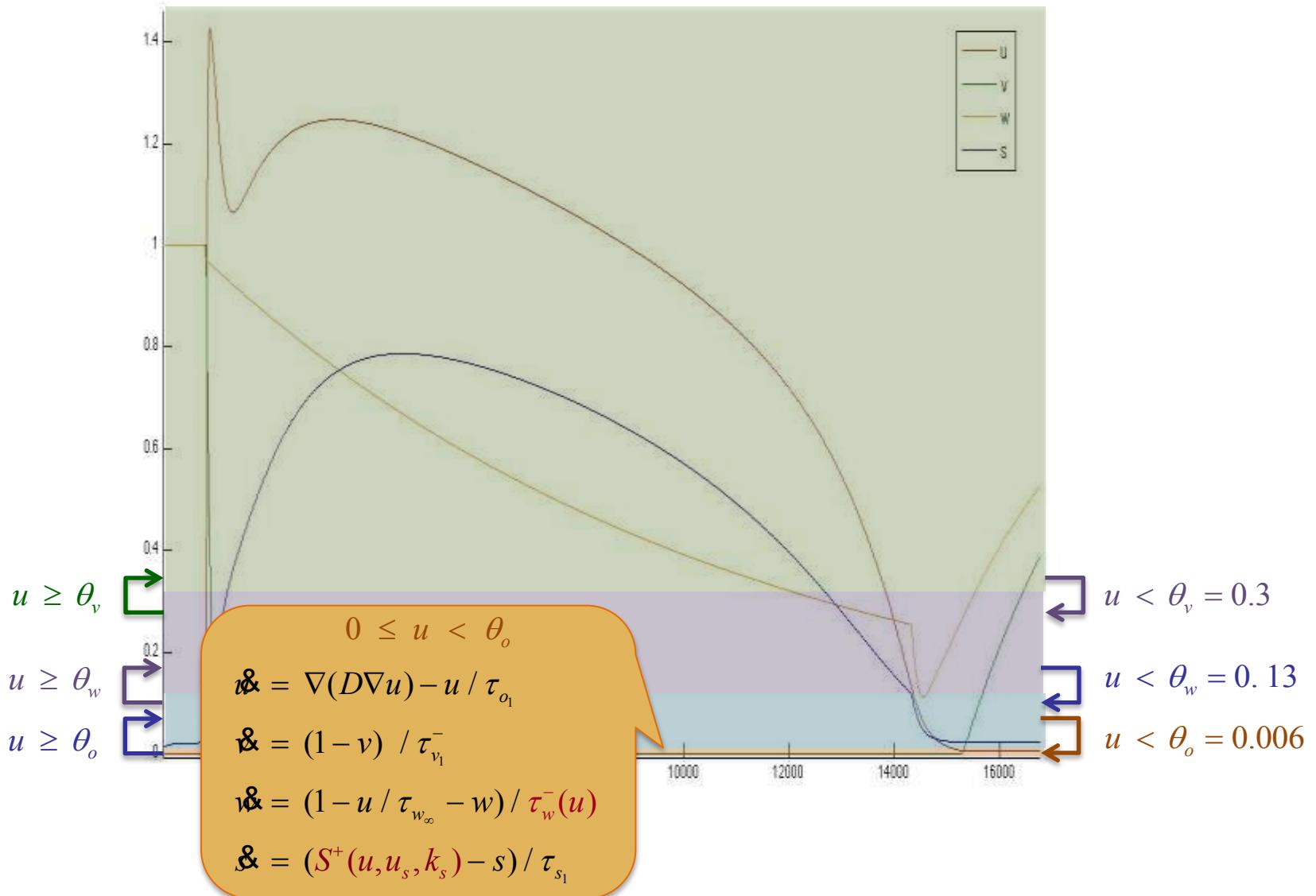
$$\tau_{so}(u) = S^+(u, u_s, k_{so}, \tau_{so_1}, \tau_{so_2})$$



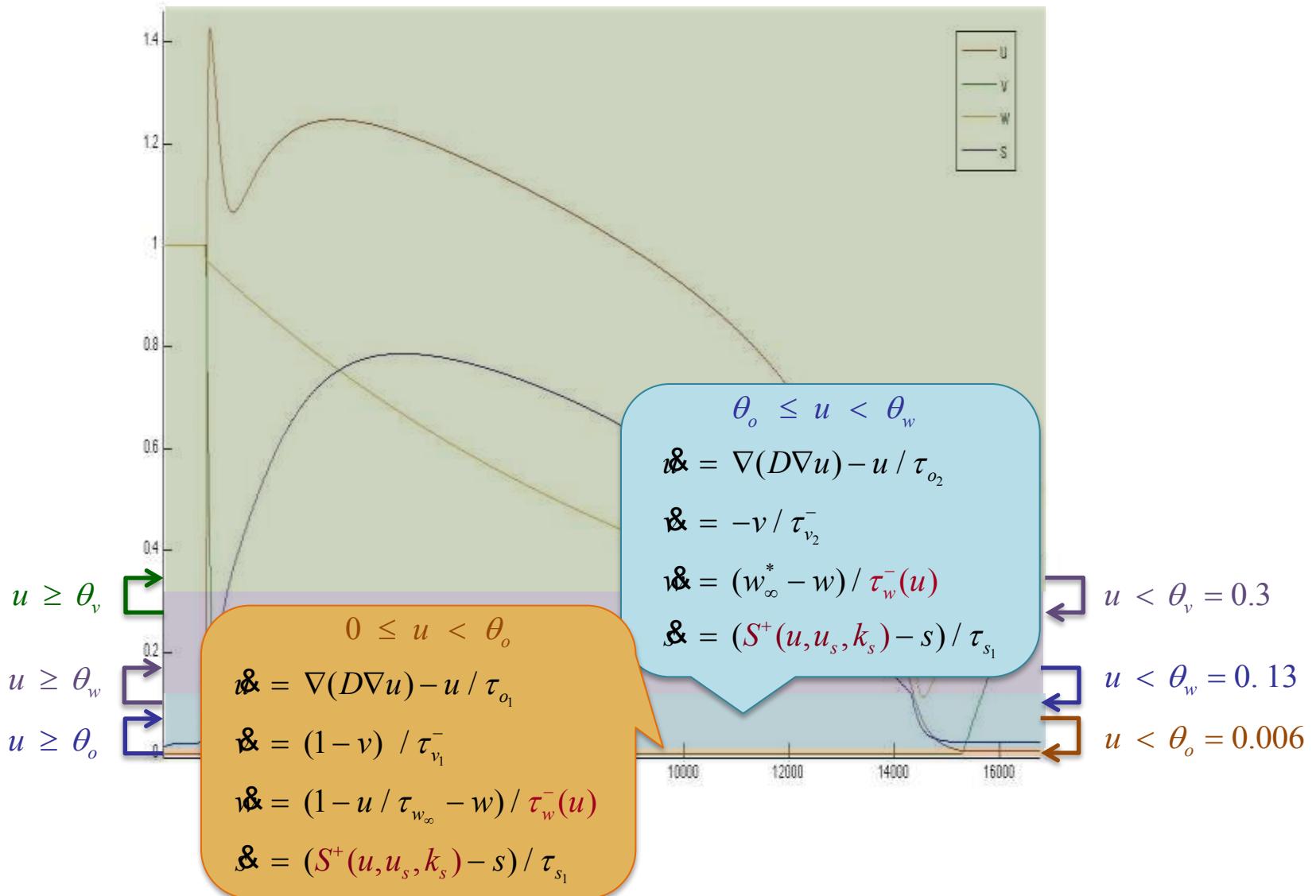
Minimal Resistance Model (MRM)



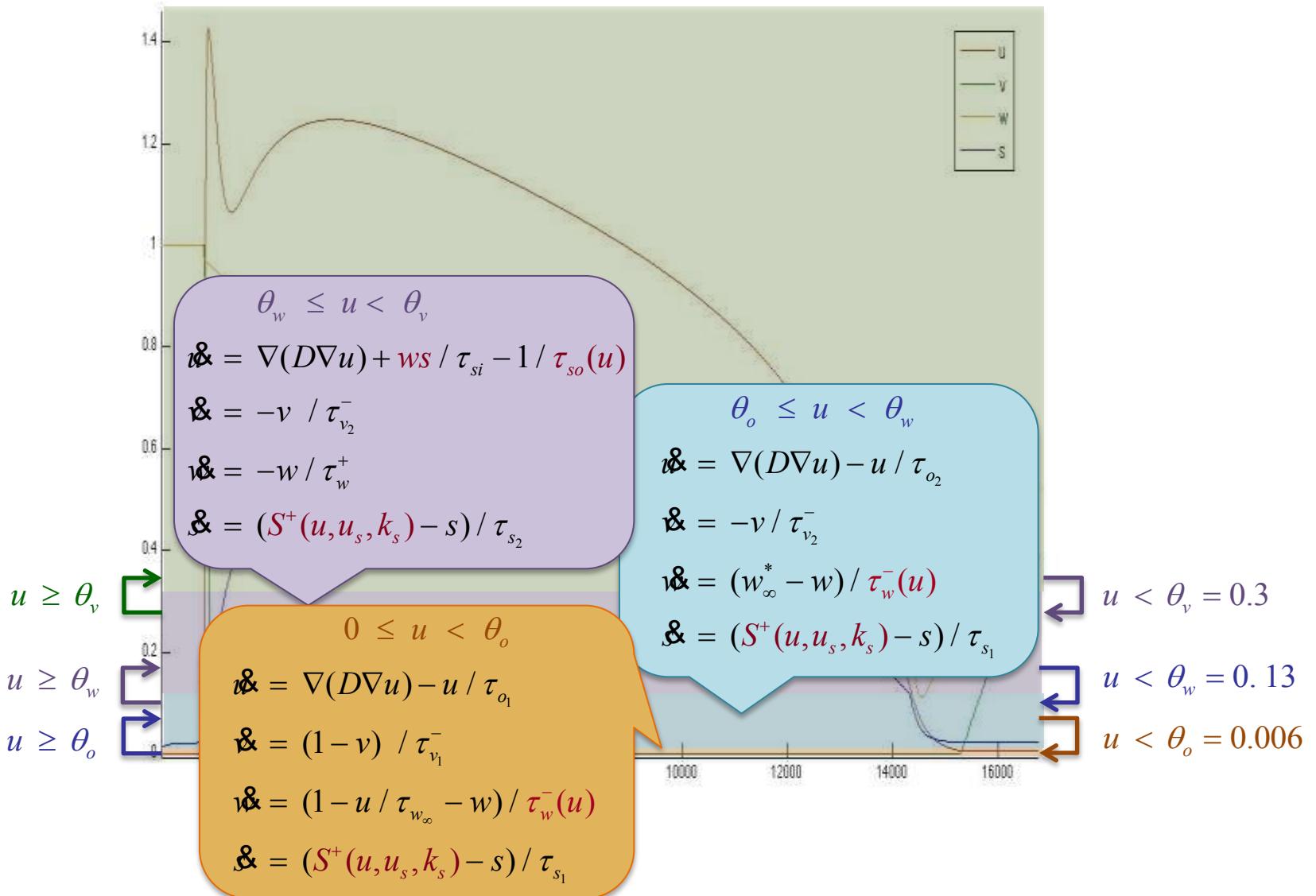
Minimal Resistance Model (MRM)



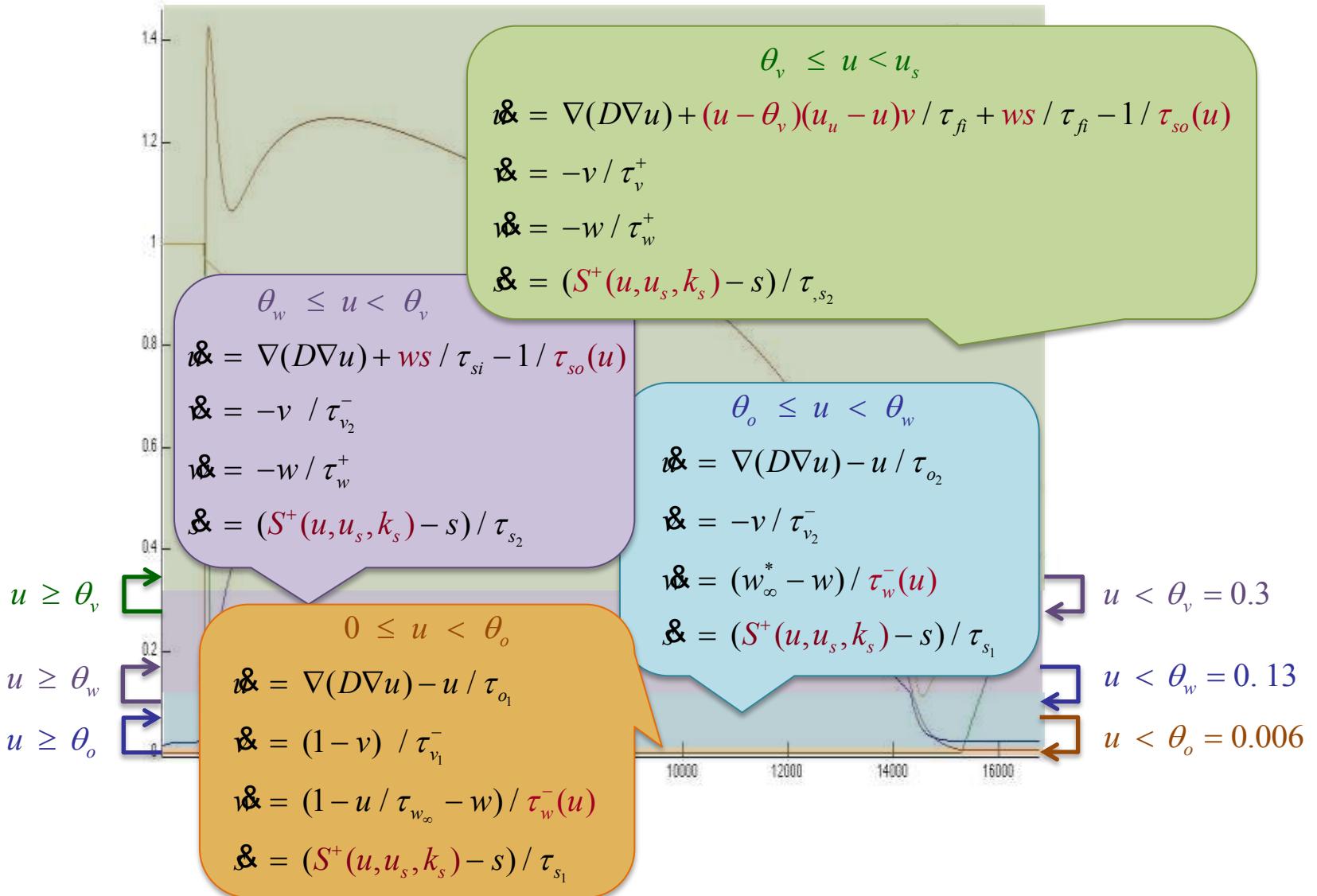
Minimal Resistance Model (MRM)



Minimal Resistance Model (MRM)



Minimal Resistance Model (MRM)



Sigmoid Closure Property

Theorem: For $ab > 0$, scaled sigmoids are closed under the reciprocal operation:

$$S^+(u, k, \theta, a, b)^{-1} = S^-(u, k, \theta + \frac{\ln(\frac{a}{b})}{2k}, \frac{1}{b}, \frac{1}{a})$$

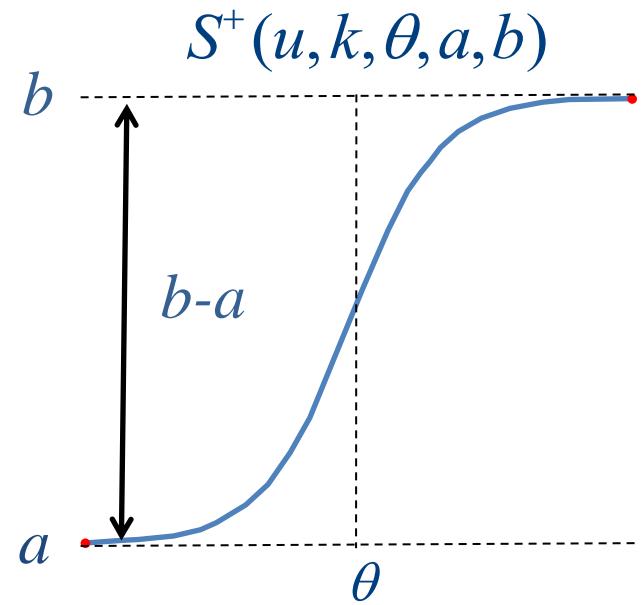
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Proof:

$$S^+(u, k, \theta, a, b)^{-1} = \left(a + \frac{b-a}{1+e^{-2k(u-\theta)}} \right)^{-1}$$



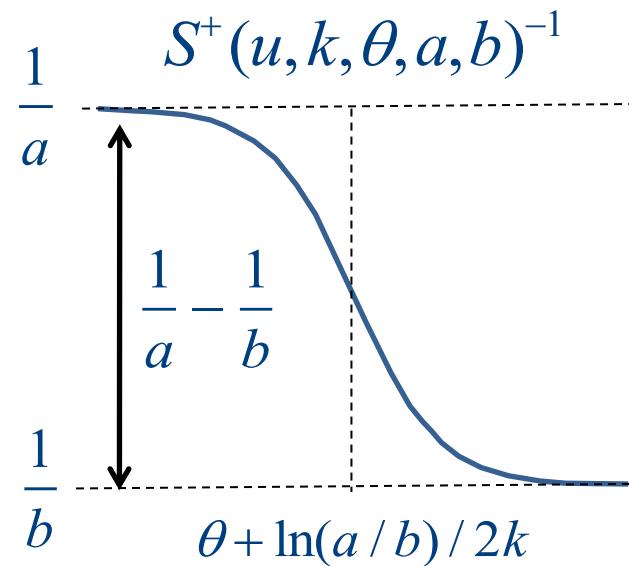
Sigmoid Reciprocal Closure

Theorem: For $a^*b > 0$, scaled sigmoids are closed under the reciprocal operation:

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Proof:

$$S^+(u, k, \theta, a, b)^{-1} = \frac{1}{a} - \frac{\frac{1}{a} - \frac{1}{b}}{1 + e^{-2k(u - (\theta + \frac{\ln a - \ln b}{2k}))}}$$



From Resistances to Conductances

Removing Divisions using Sigmoid Reciprocal:

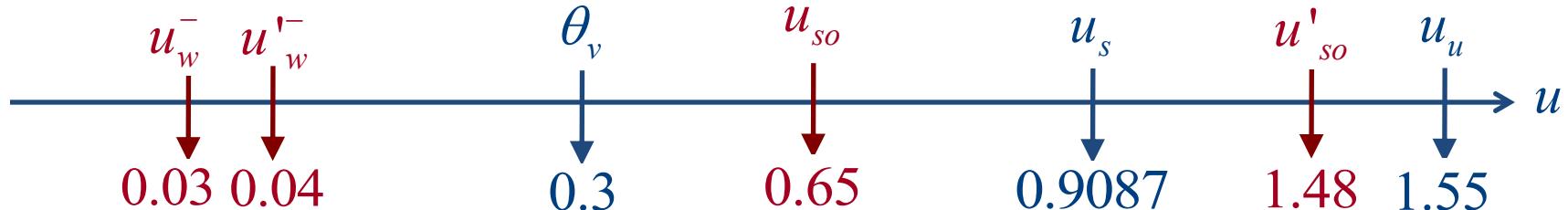
$$\tau_w^- = S^-(u, k_w^-, \textcolor{red}{u}_w^-, \tau_{w_1}^-, \tau_{w_2}^-) \quad g_w^- = 1 / \tau_w^- = S^+(u, k_w^-, \textcolor{red}{u}_w^-, \tau_{w_1}^{-1}, \tau_{w_2}^{-1})$$



From Resistances to Conductances

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From Resistances to Conductances

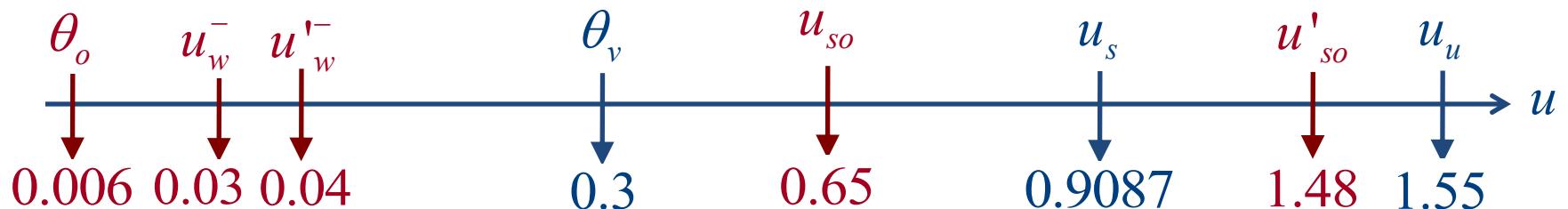
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Removing Divisions using Step Reciprocal:

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$$v_\infty = H^-(u, \theta_o, 0, 1) \quad w_\infty = H^-(u, \theta_o, 0, 1) (1 - ug_{w\infty}) + H^+(u, \theta_o, 0, w_\infty^*)$$



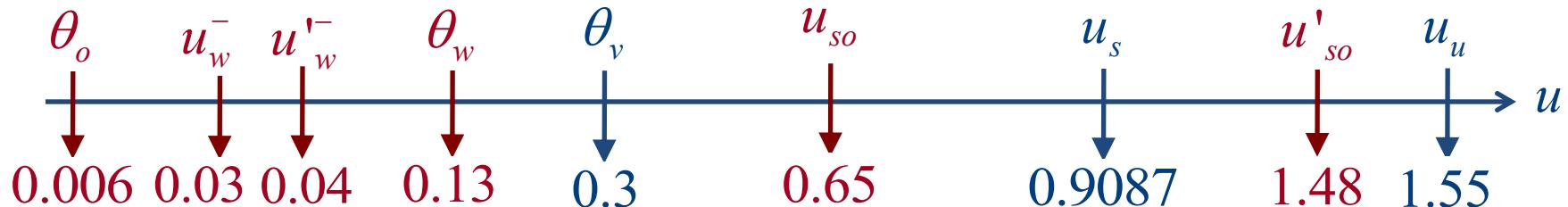
From Resistances to Conductances

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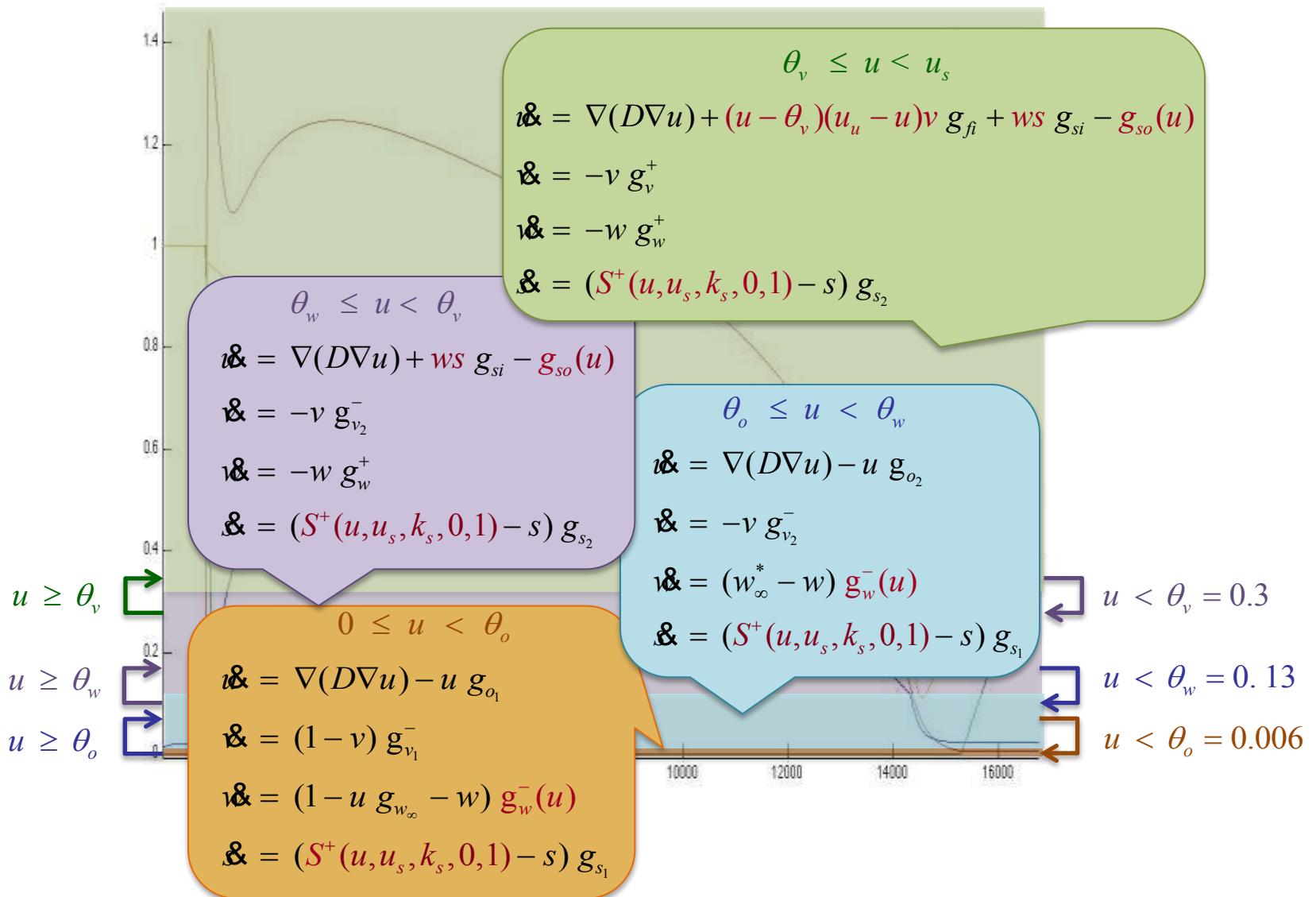
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Minimal Conductance Model (MCM)



Gene Regulatory Networks (GRN)

GRN canonical sigmoidal form:

$$\dot{u}_i = \sum_{j=1}^{m_i} a_{ij} \prod_{k=1}^{n_j} S^\pm(u_k, k_k, \theta_k, a_k, b_k) - b_i u_i$$

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a_{ij} : are activation / inhibition constants

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Note: steps and ramps are sigmoid approximations

Optimal Polygonal Approximation

Given: One nonlinear curve and desired # segments

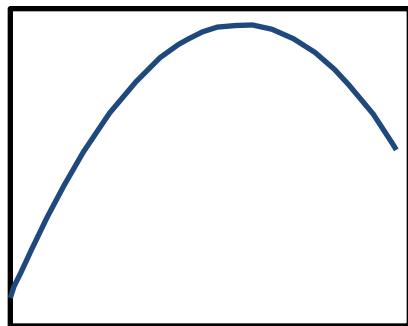
Find: Optimal polygonal approximation

Optimal Polygonal Approximation

Given: One nonlinear curve and desired # segments

Find: Optimal polygonal approximation

Example: What is the optimal polygonal approximation of the blue curve with 3 segments ?

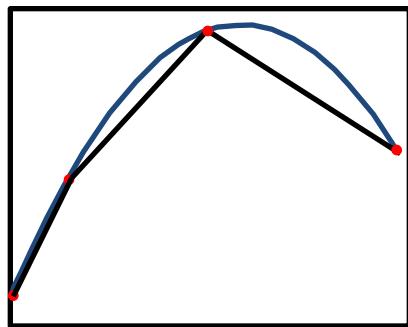


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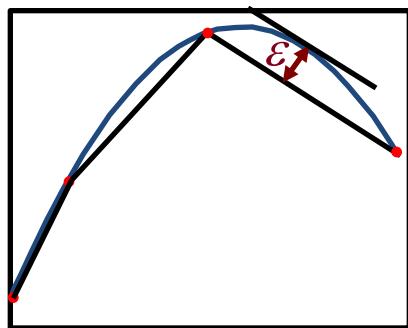


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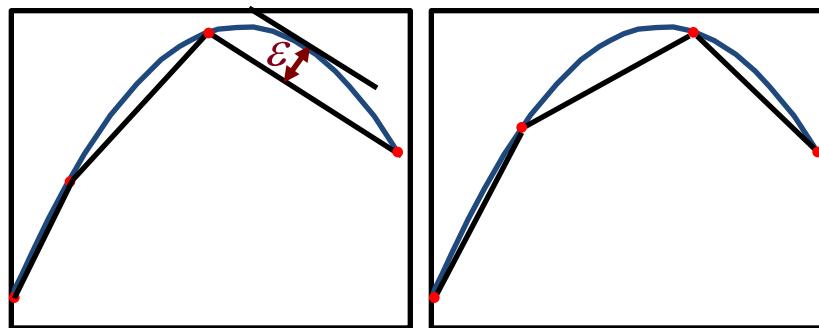


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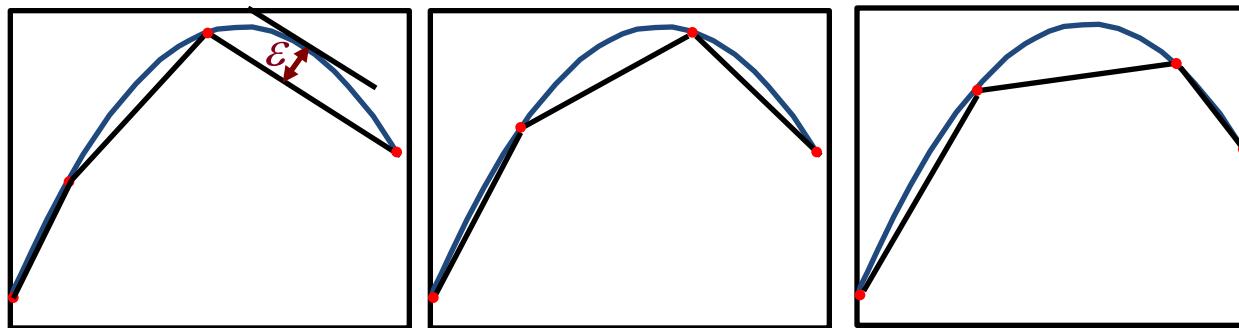


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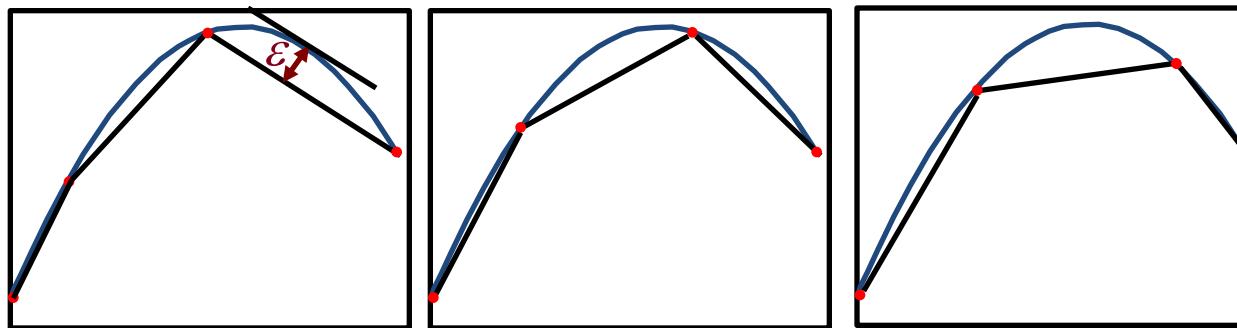


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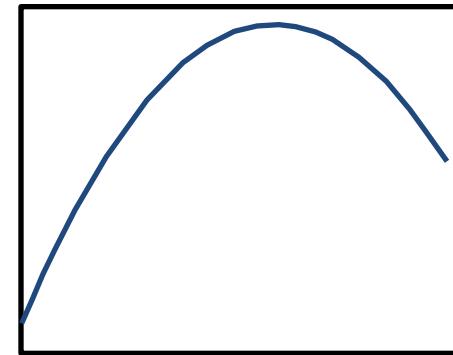
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Dynamic Programming Algorithm

- **Complexity:** $O(P^2)$
- **P:** # points of the curve

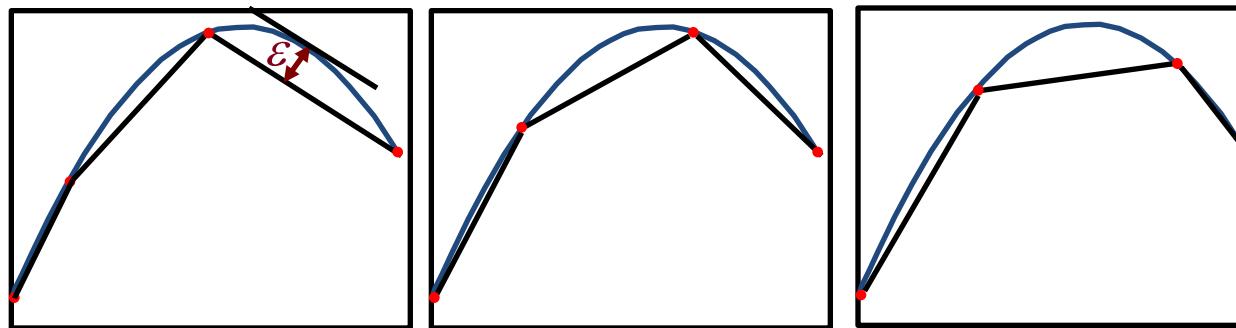


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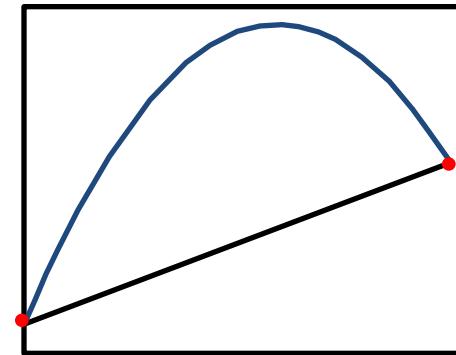
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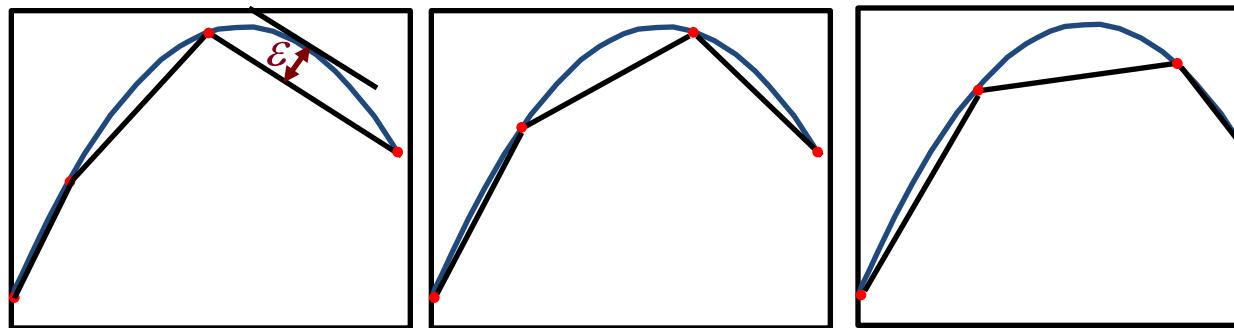


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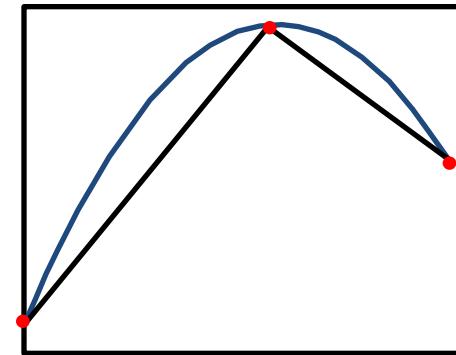
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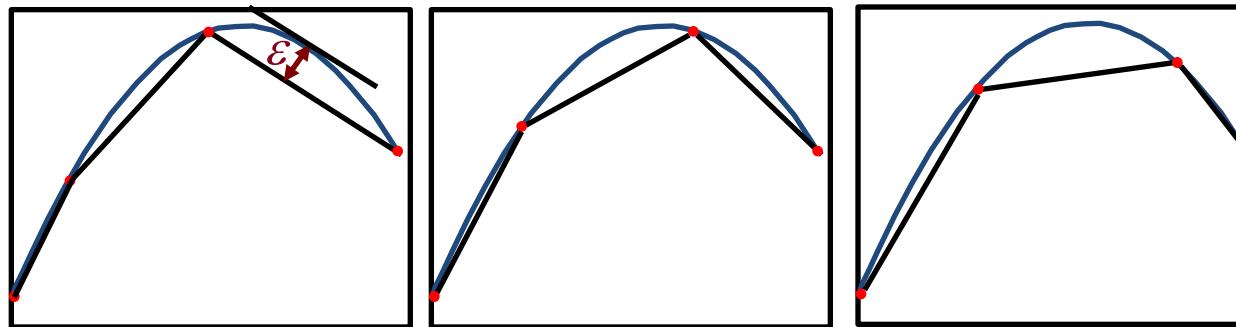


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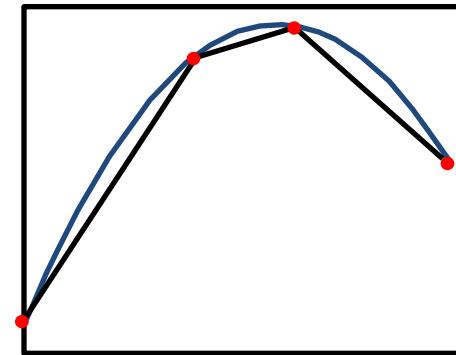
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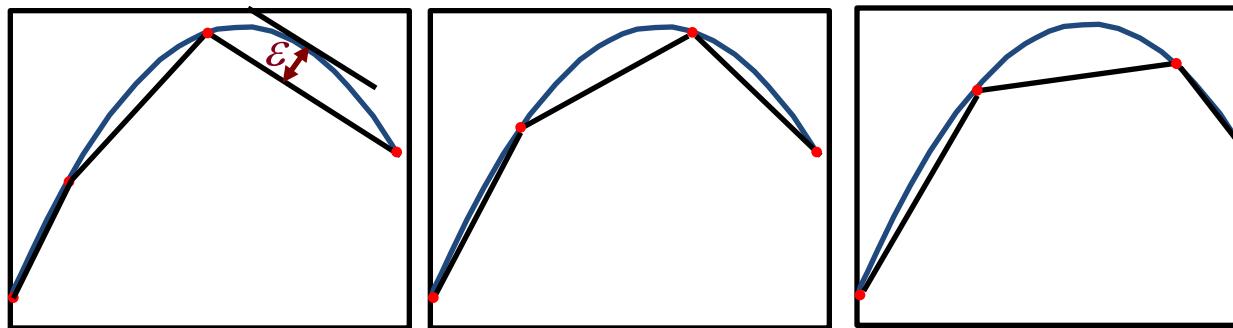


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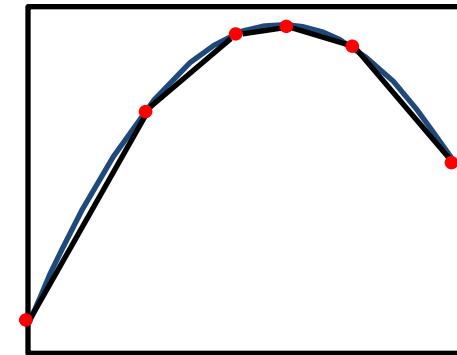
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Dynamic Programming Algorithm

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Globally-Optimal Polygonal Approximation

Given: Set of nonlinear curves **and** desired # of segments

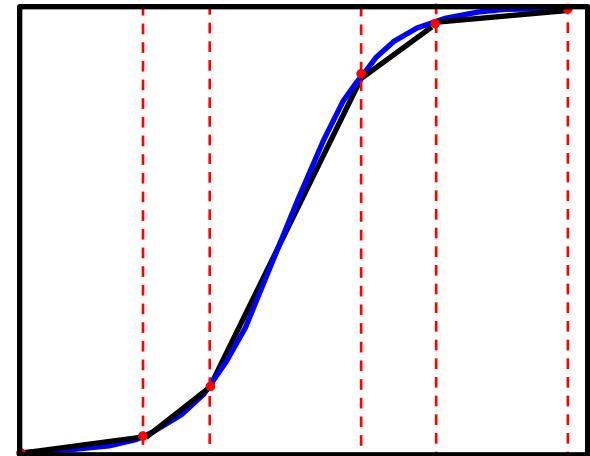
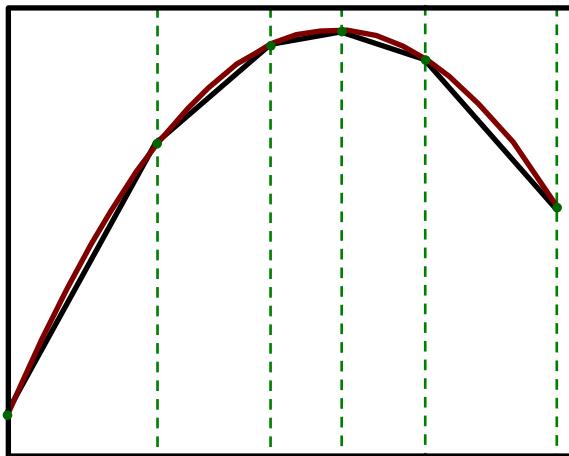
Find: Globally optimal polygonal approximation

Globally-Optimal Polygonal Approximation

Given: Set of nonlinear curves and desired # of segments

Find: Globally optimal polygonal approximation

Example: What is the optimal polygonal approximation of the curves below with 5 segments ?

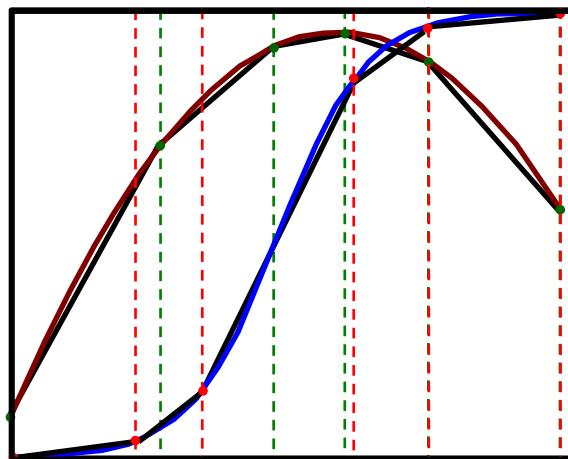


Globally-Optimal Polygonal Approximation

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Example: What is the optimal polygonal approximation of the curves below with 5 segments ?



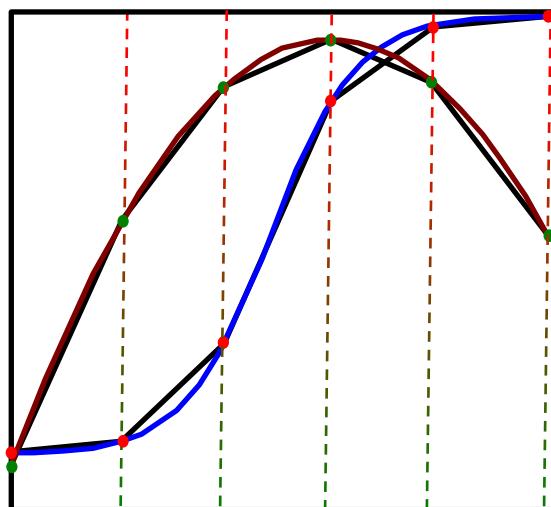
Combining the two we obtain 8 segments and not 5 segments

Globally-Optimal Polygonal Approximation

Given: Set of nonlinear curves and desired # of segments

Find: Globally optimal polygonal approximation

Example: What is the optimal polygonal approximation of the curves below with 5 segments ?



Solution: modify the OPAA to minimize the maximum error of a set of curves simultaneously.

Deriving the Piecewise Multi-Affine Model

$$(\theta_v \leq u < u_u)$$

$$\dot{v} = e + (u - \theta_v)(u_u - u)v g_{fi} + ws g_{si} - g_{so}(u)$$

$$\dot{w} = -v g_v^+$$

$$\dot{s} = -w g_w^+$$

$$\dot{e} = S^+(u, k_s, u_s, 0, 1) g_{s_2} - s g_{s_2}$$

$$\begin{cases} u < \theta_v \\ u \geq \theta_v \end{cases}$$

$$\theta_w \leq u < \theta_v$$

$$\dot{v} = e + ws g_{si} - g_{so}(u)$$

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$$\theta_o \leq u < \theta_w$$

$$\dot{v} = e - u g_{o_2}$$

$$\dot{w} = -v g_{v_2}^-$$

$$\dot{s} = (w_\infty^* - w) g_w^-(u)$$

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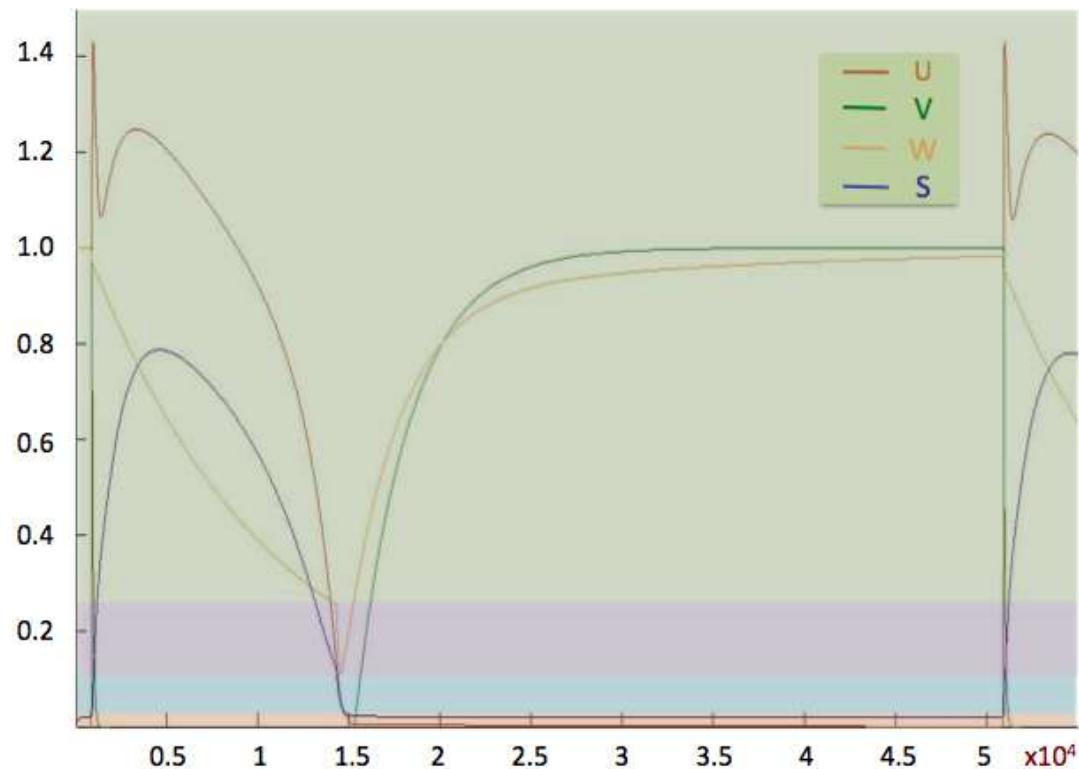
$$0 \leq u < \theta_o$$

$$\dot{v} = e - u g_{o_1}$$

$$\dot{w} = (1 - v) g_{v_1}^-$$

$$\dot{s} = (1 - u g_{w_\infty} - w) g_w^-(u)$$

$$\dot{e} = S^+(u, k_s, u_s) g_{s_1} - s g_{s_1}$$



Deriving the Piecewise Multi-Affine Model

$$(\theta_v \leq u < u_u)$$

$$\dot{e} = e + (u - \theta_v)(u_u - u)v g_{fi} + ws g_{si} - g_{so}(u)$$

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$$\theta_w \leq u < \theta_v$$

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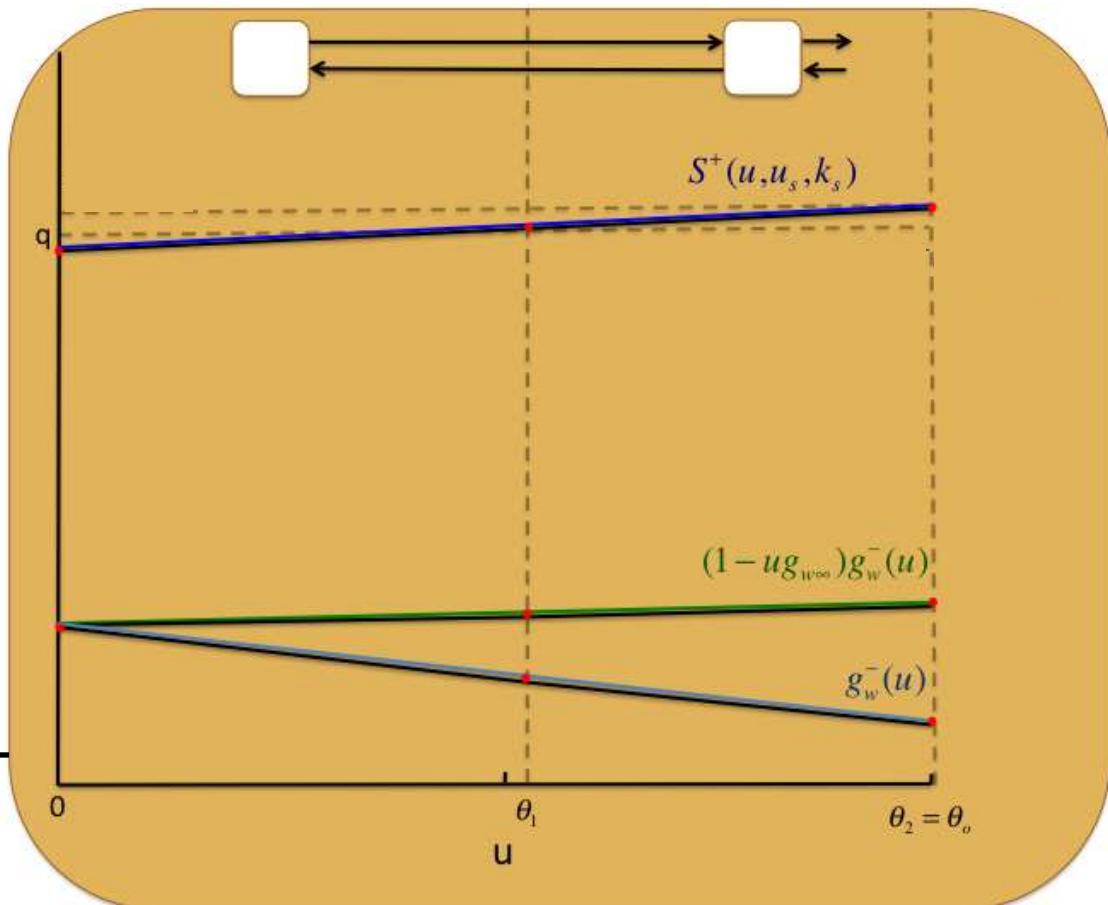
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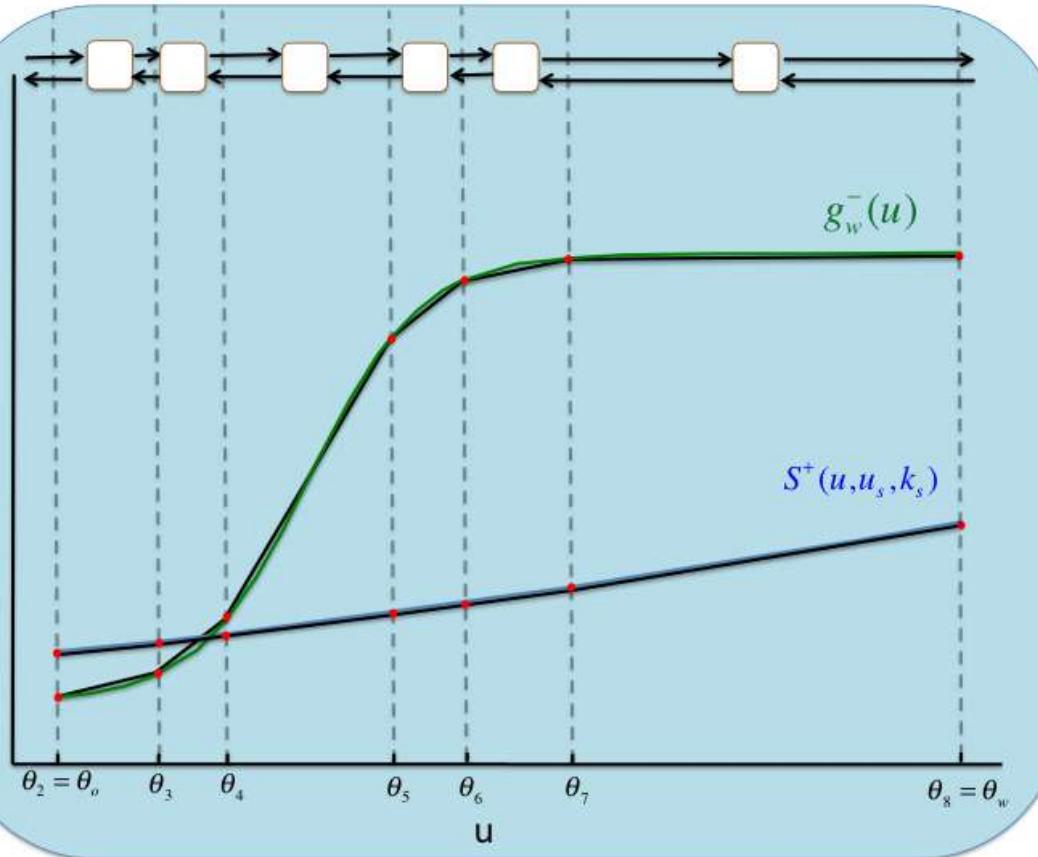
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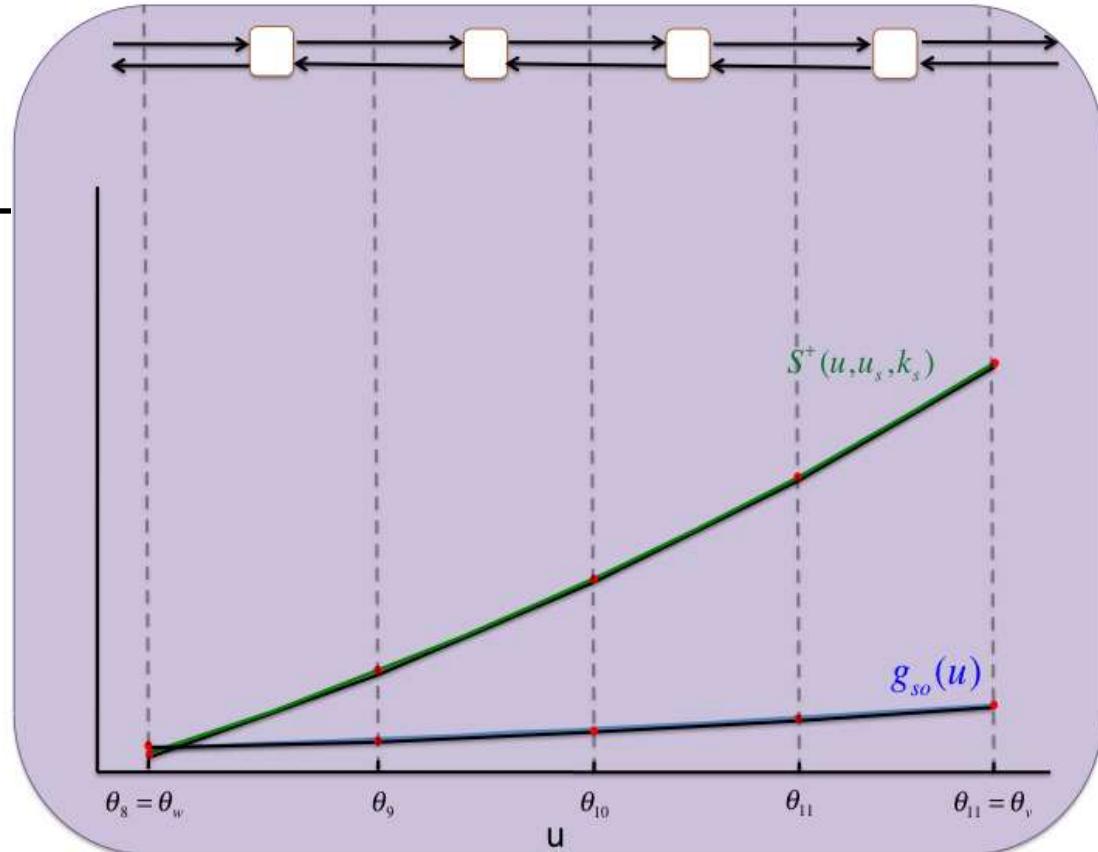
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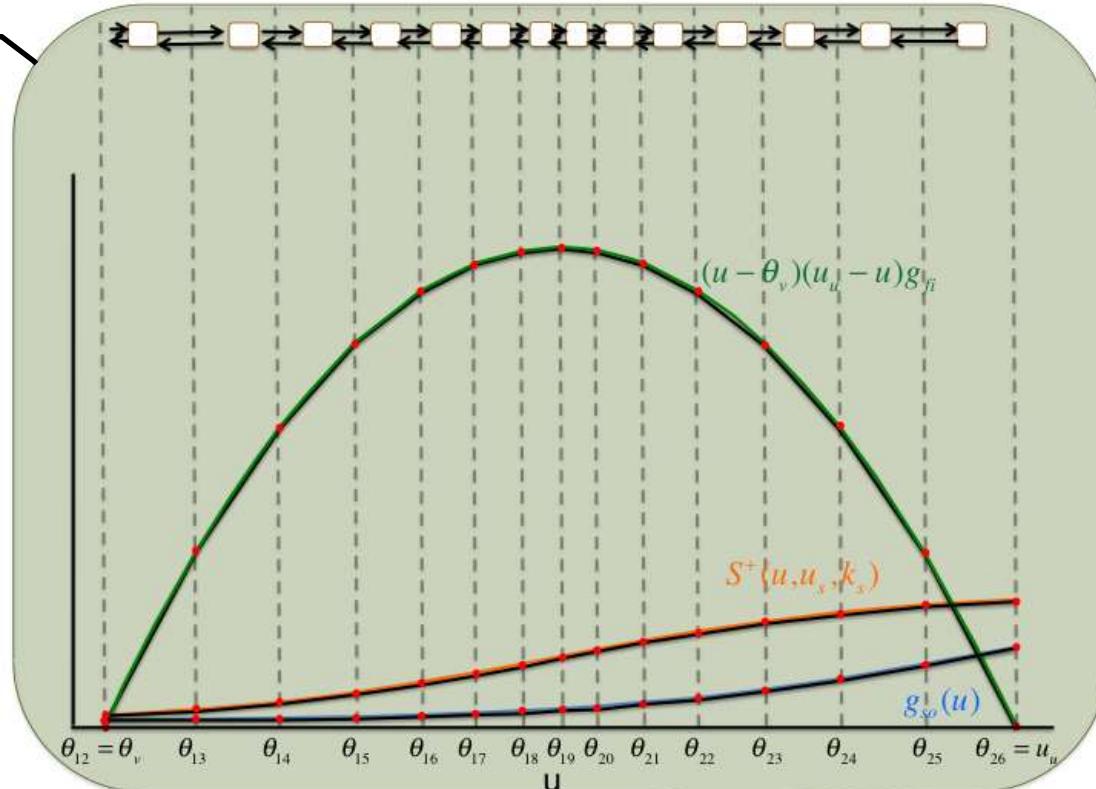
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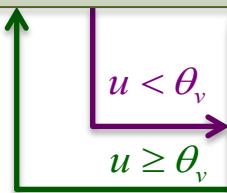
$$\theta_{12} = \theta_v < u \leq u_u = \theta_{26}$$

$$i\& = e + \sum_{i=12}^{25} R(u, \theta_i, \theta_{i+1}, u_{f_i}, u_{f_{i+1}}) v g_{fi} + ws g_{si} - \sum_{i=12}^{25} R(u, \theta_i, \theta_{i+1}, u_{so_i}, u_{so_{i+1}}) g_{so}$$

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$$s\& = (\sum_{i=12}^{25} R(u, \theta_i, \theta_{i+1}, u_{s_i}, u_{s_{i+1}}) - s) g_{s_2}$$



$$\theta_8 = \theta_w \leq u < \theta_v = \theta_{12}$$

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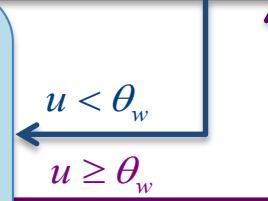
$$\theta_2 = \theta_o \leq u < \theta_w = \theta_8$$

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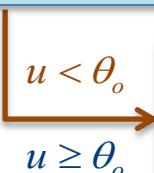
$$\theta_0 = 0 \leq u < \theta_o = \theta_2$$

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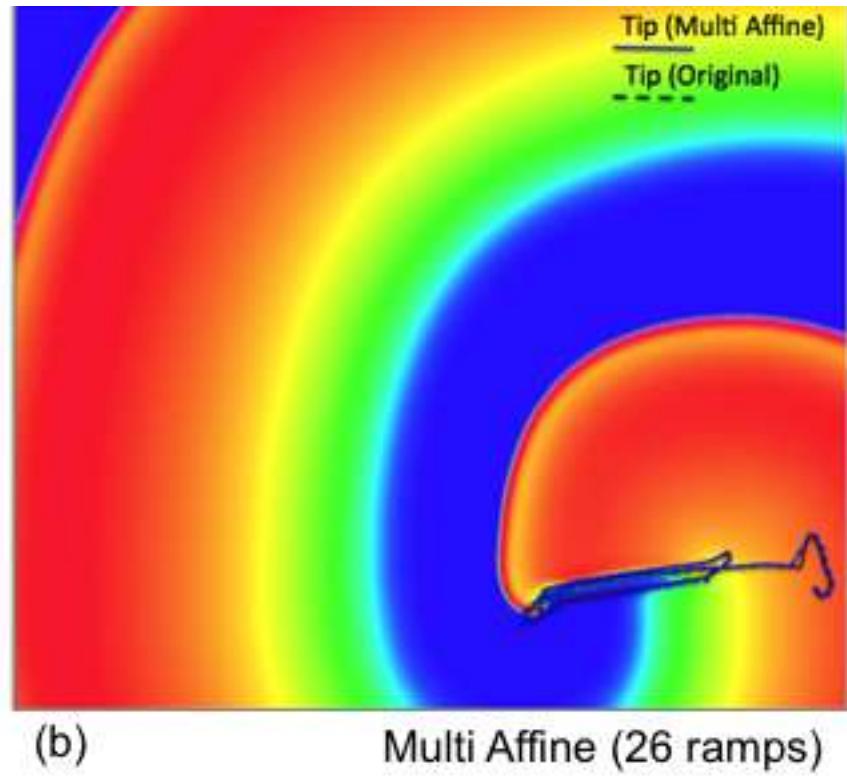
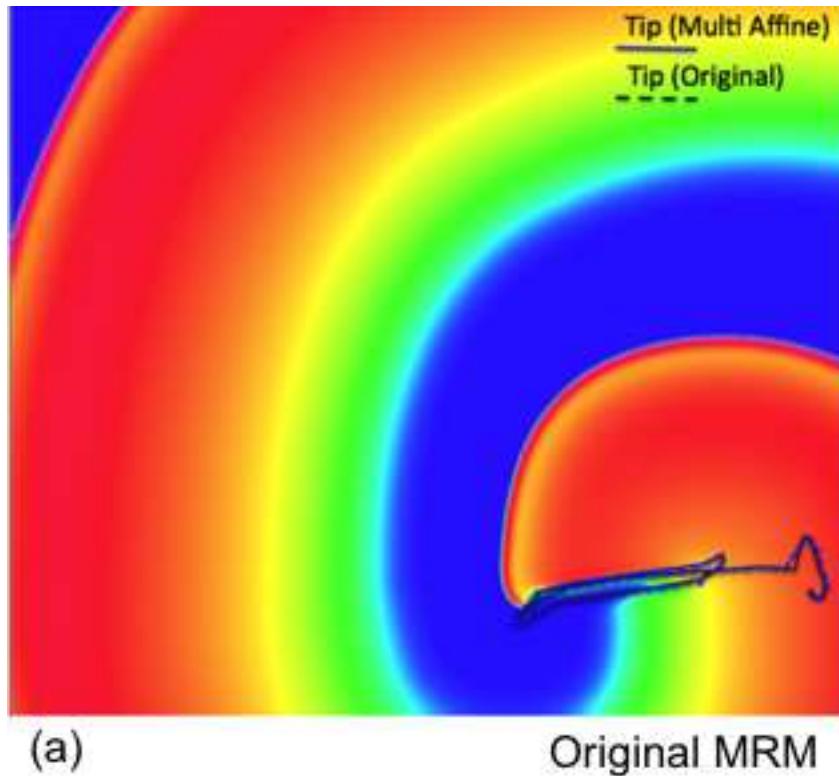
$$v\& = (1 - v) g_{v_1}^-$$

$$w\& = (\sum_{i=0}^1 (R(u, \theta_i, \theta_{i+1}, u_{w_i}^+, u_{w_{i+1}}^+) - w R(u, \theta_i, \theta_{i+1}, u_{w_i}^-, u_{w_{i+1}}^-)) g_{w_a}$$

$$s\& = (\sum_{i=0}^1 R(u, \theta_i, \theta_{i+1}, u_{s_i}, u_{s_{i+1}}) - s) g_{s_1}$$



2D Comparison



Analysis Problem

- Find parameter ranges reproducing non-excitability:
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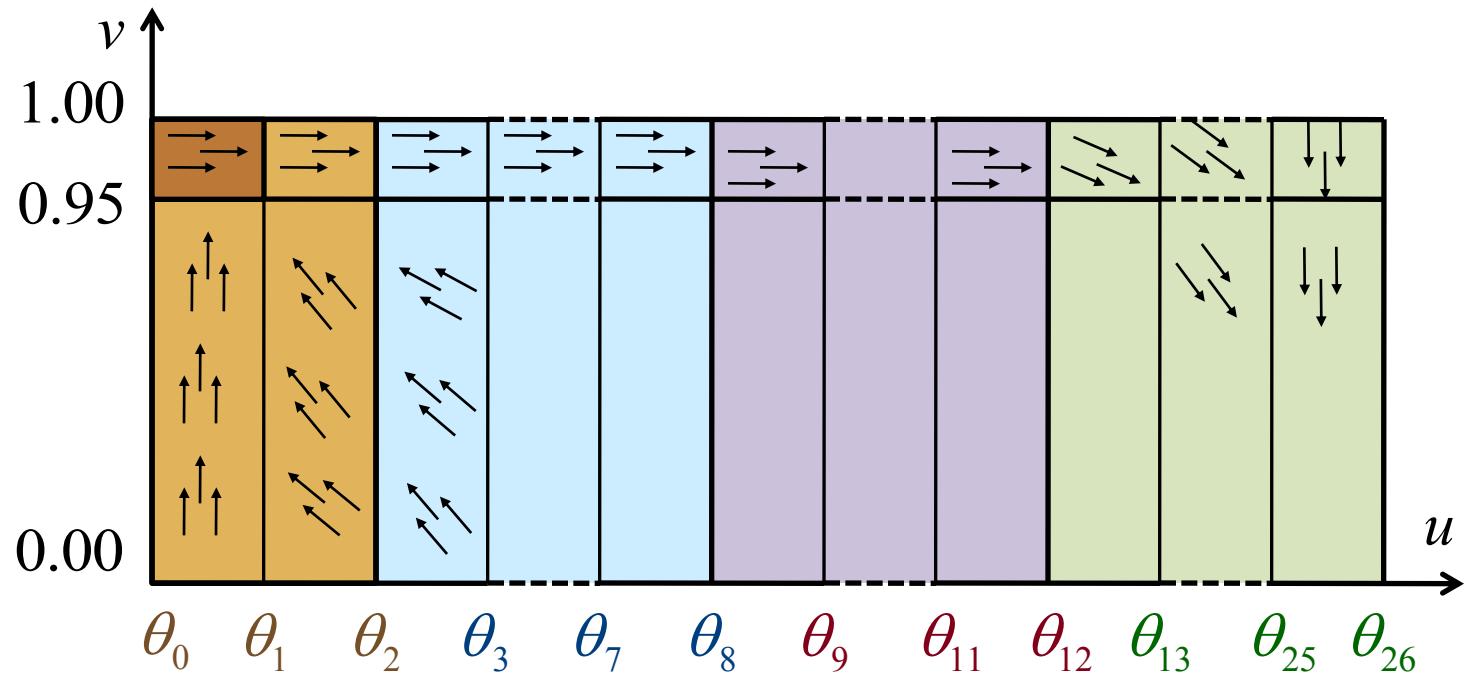
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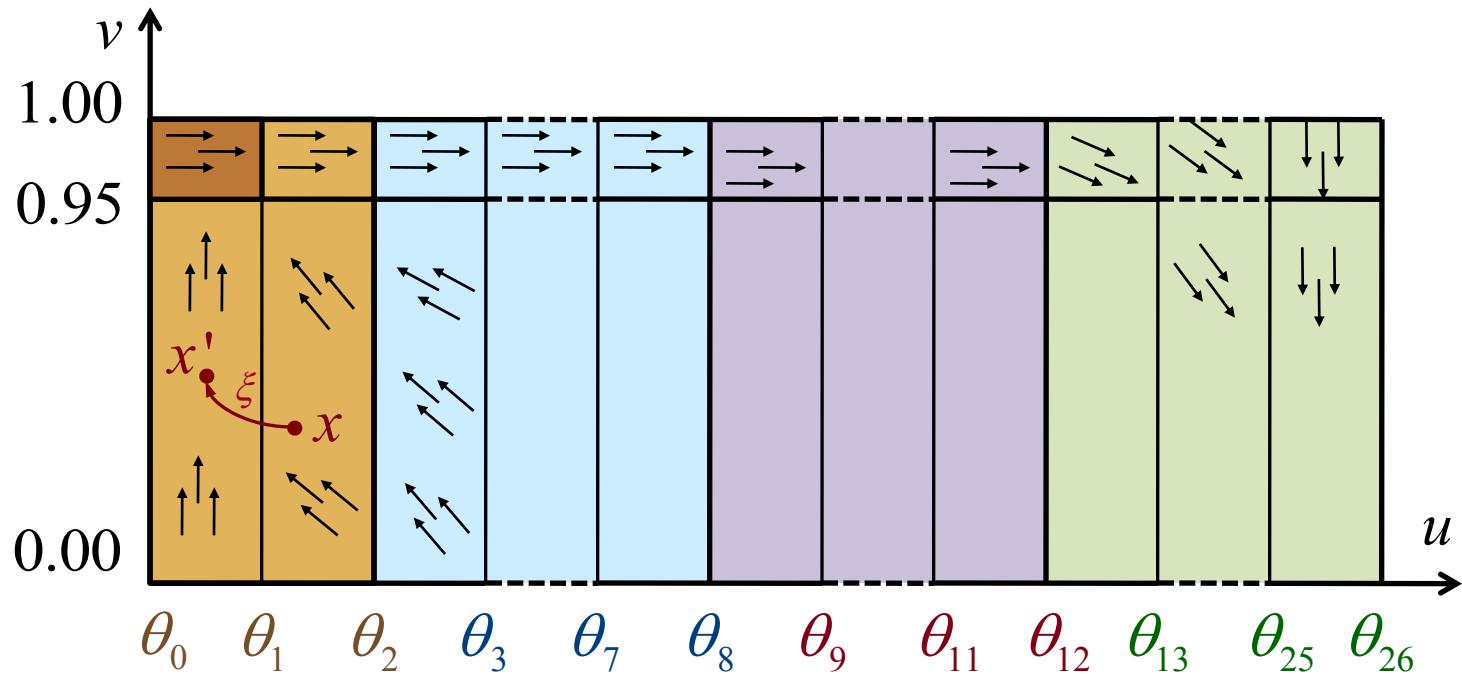
- Stimulus: $e = 1$

State Space Partition



- **Hyperrectangles:** 4 dimensional (uv-projection)
 - **Arrows:** indicate the **vector field**

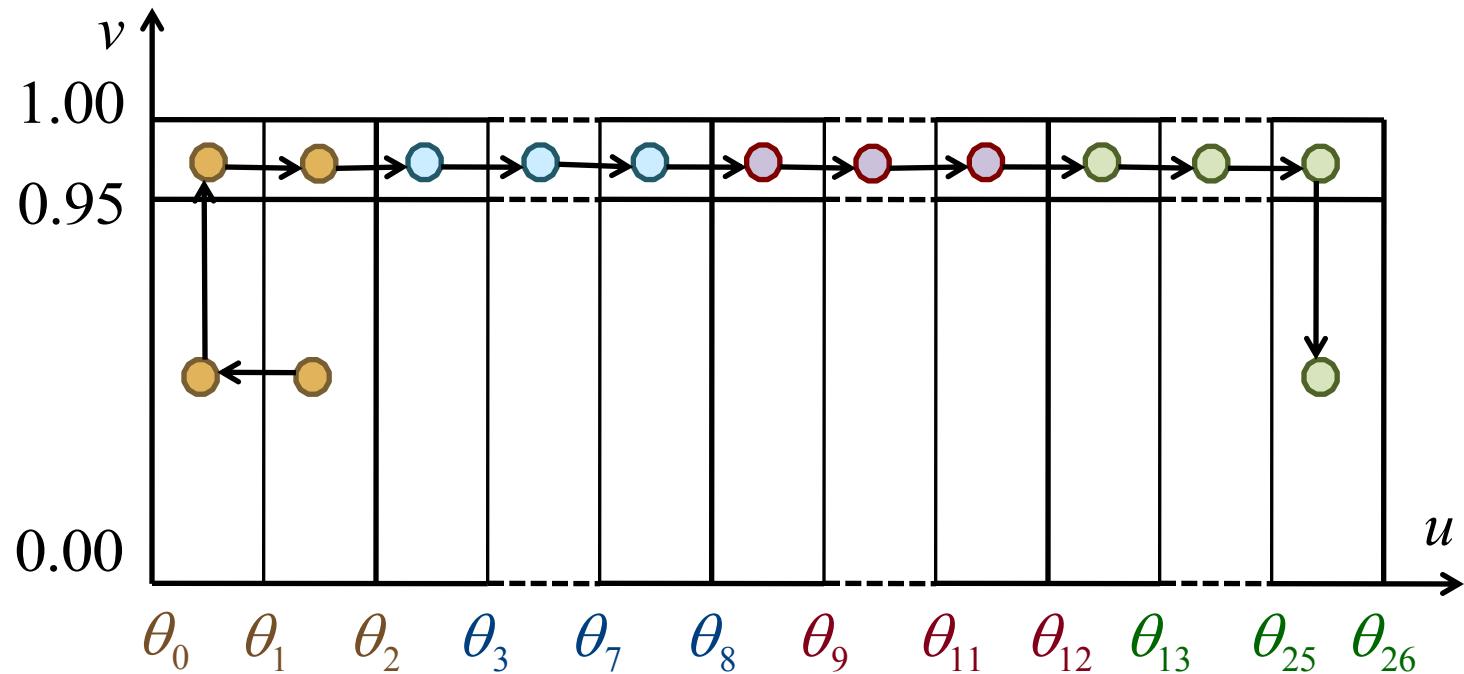
Embedding Transition System $T_X(p)$



$x \xrightarrow{T_X(p)} x'$ iff there is a solution ξ and time τ such that:

- $\xi(0) = x, \quad \xi(\tau) = x'$
- $\forall t \in [0, \tau]. \quad \xi(t) \in rect(x) \cup rect(x')$
- $rect(x)$ is adjacent to $rect(x')$

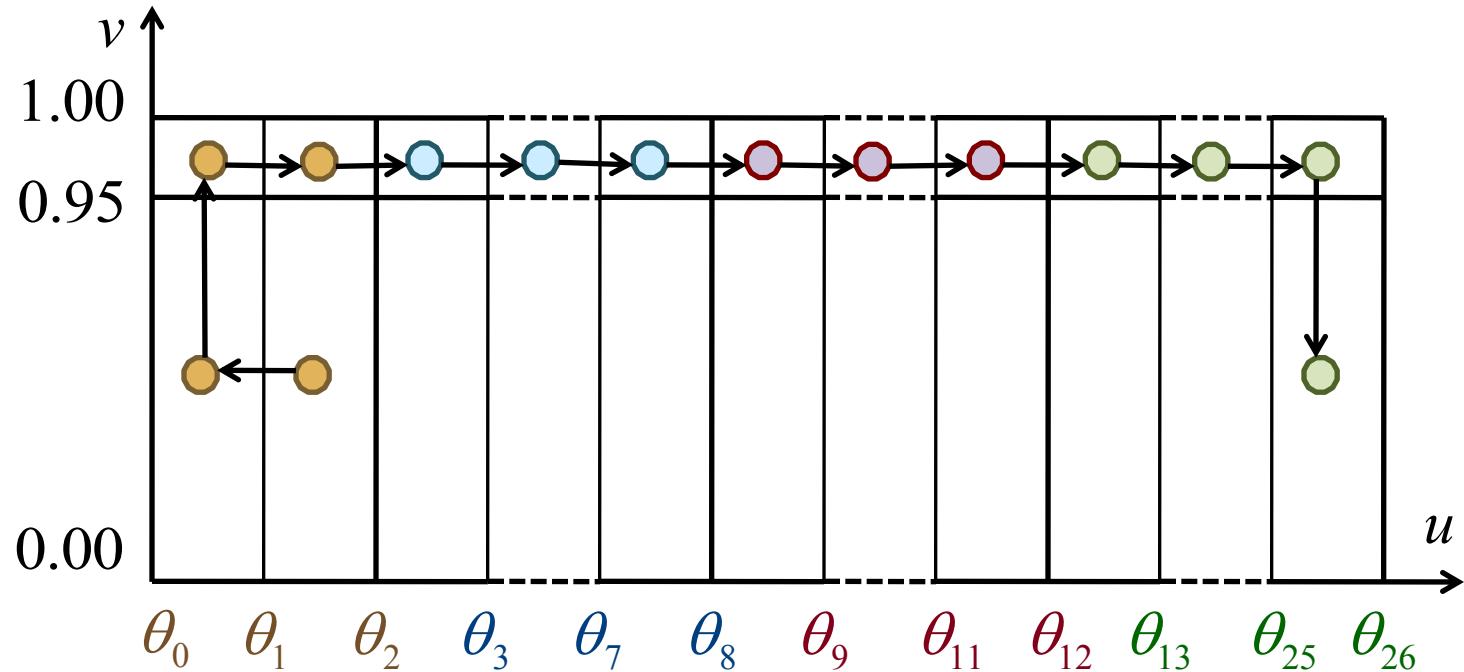
The Discrete Abstraction $T_R(p)$



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$T_R(p)$ is the quotient of $T_X(p)$ with respect to $:_{R(p)}$

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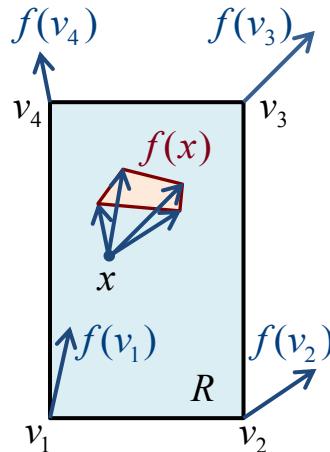


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Theorem: $\forall p. \quad T_X(p) \leq T_R(p)$

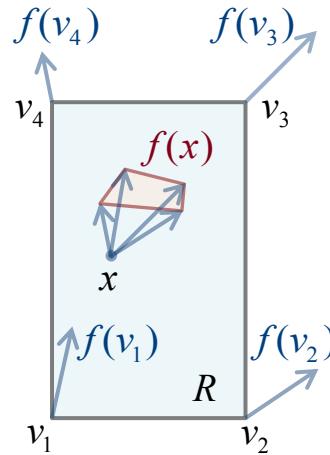
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Theorem: If f is multi-affine then

$$\forall x \in R. f(x) \in cHull(\{f(v) \mid v \in V_R\})$$

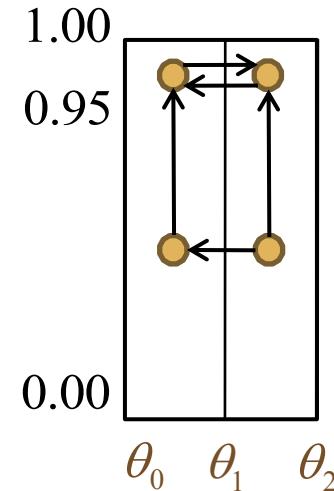
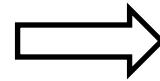
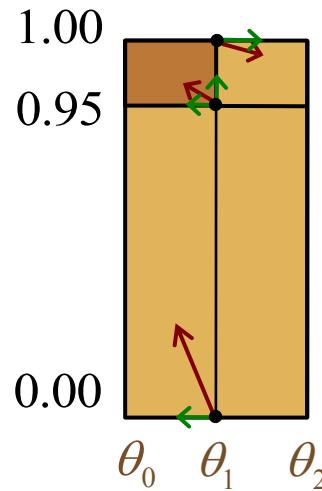
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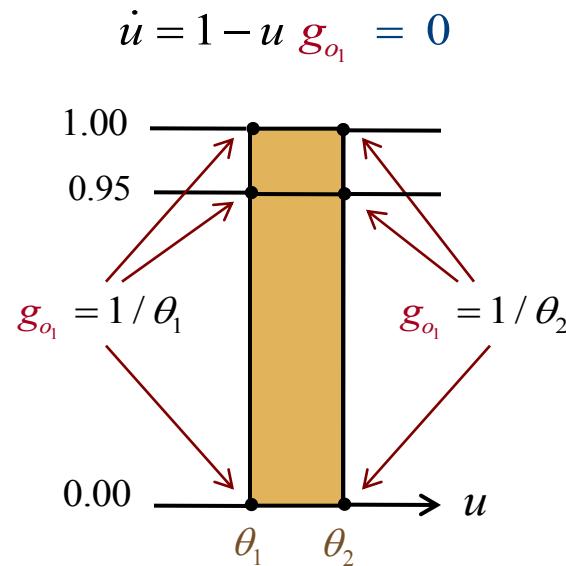
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Corollary:



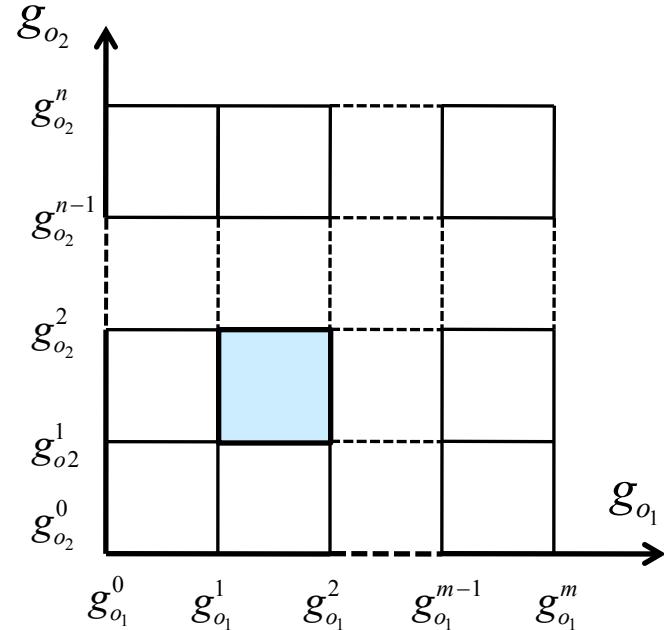
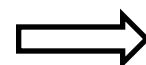
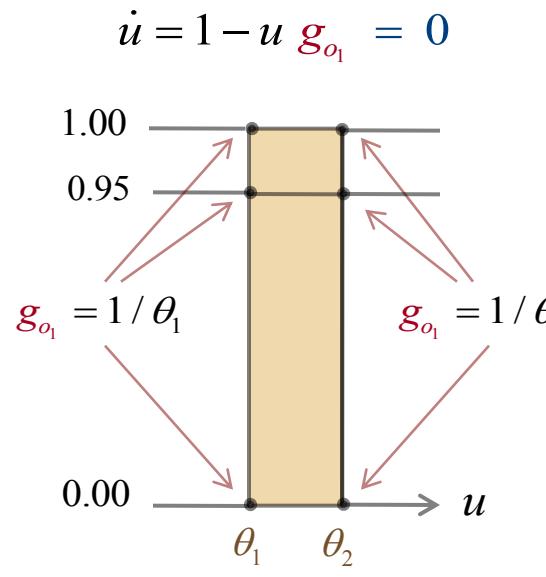
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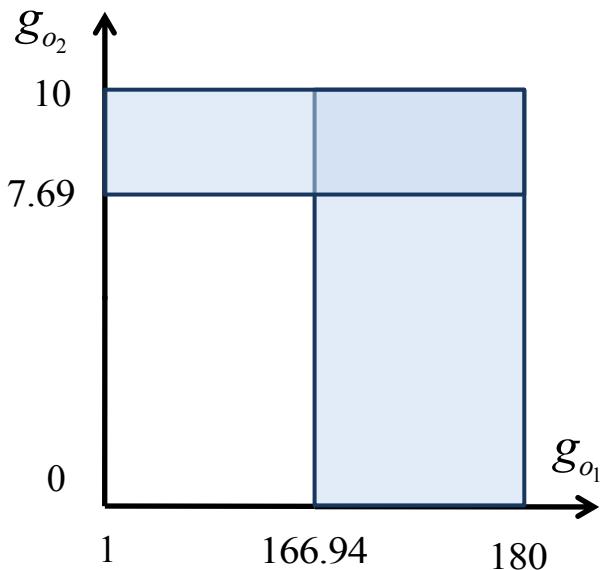
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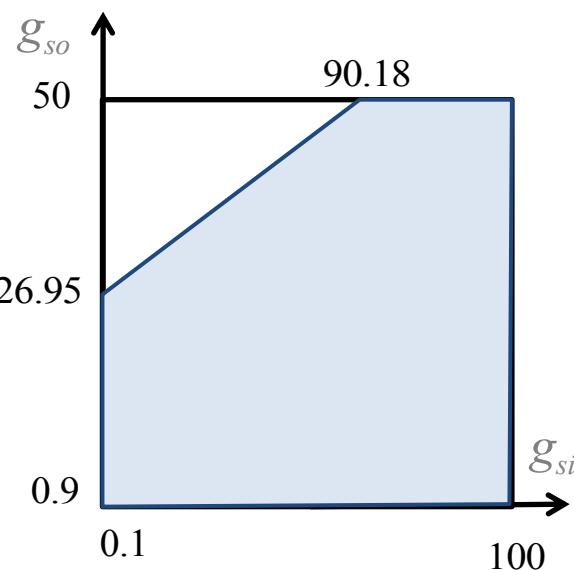
- Parameter space: 4 dimensional (g_{o_1}/g_{o_2} projection)
 - Each rectangle: a different transition system

Results

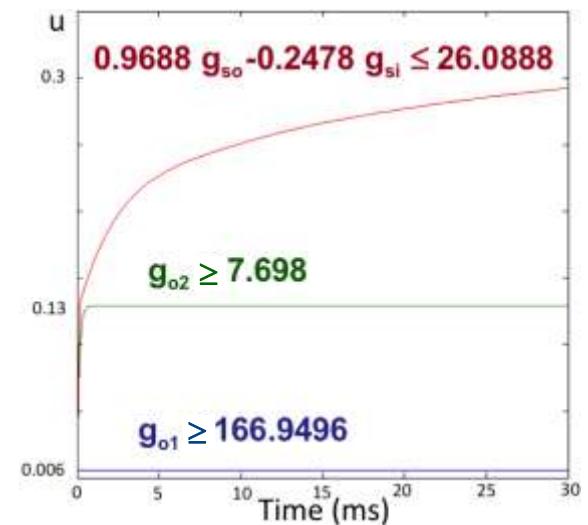
- **Rovergene: intelligently explores the PS rectangles**



independent



linearly dependent



simulation

Conclusions and Outlook

- First automatic parameter-range identification for CC
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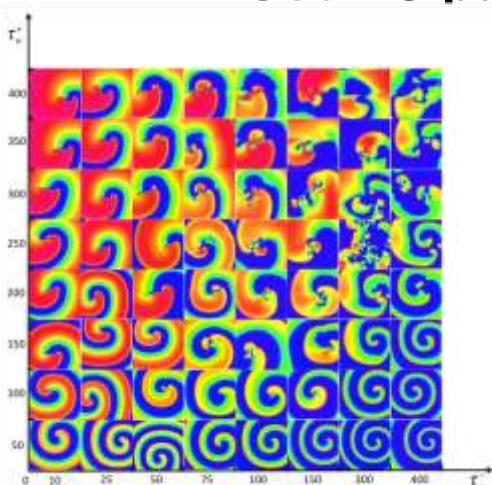
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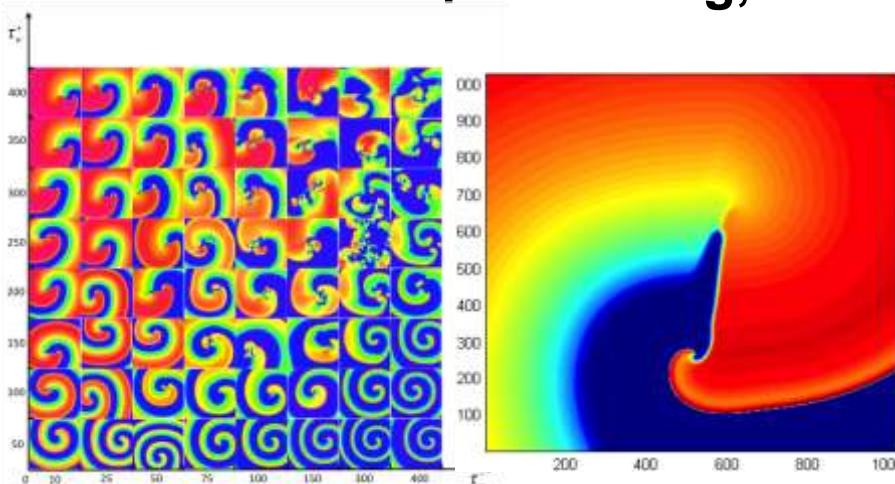
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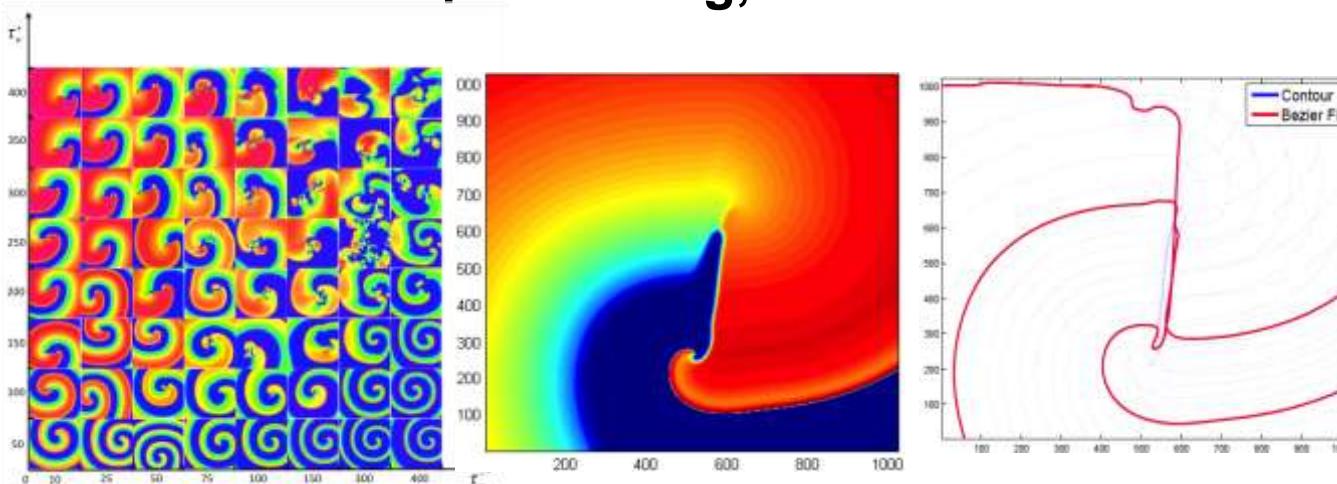
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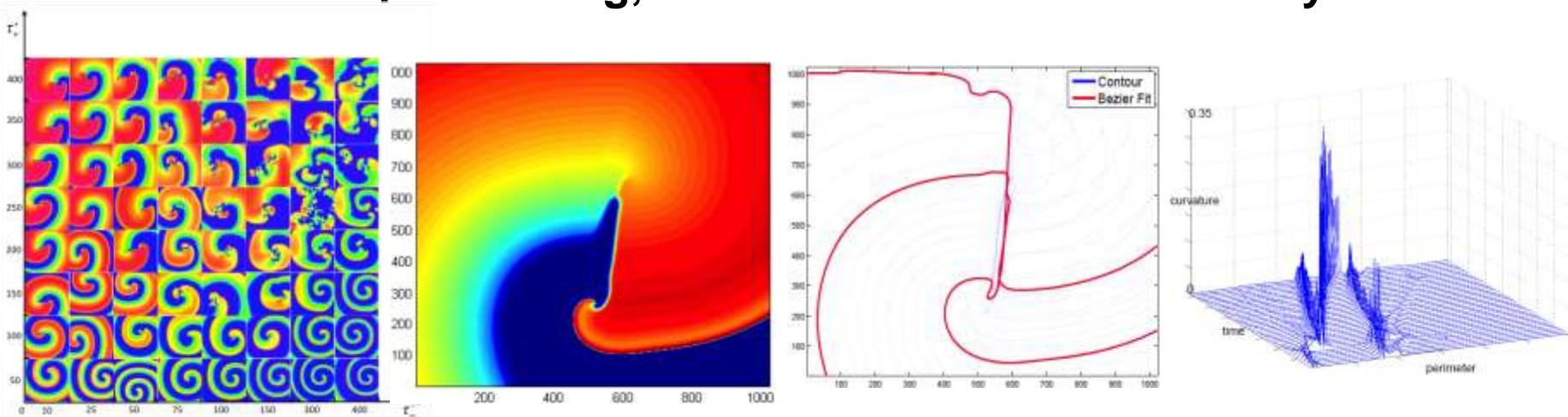
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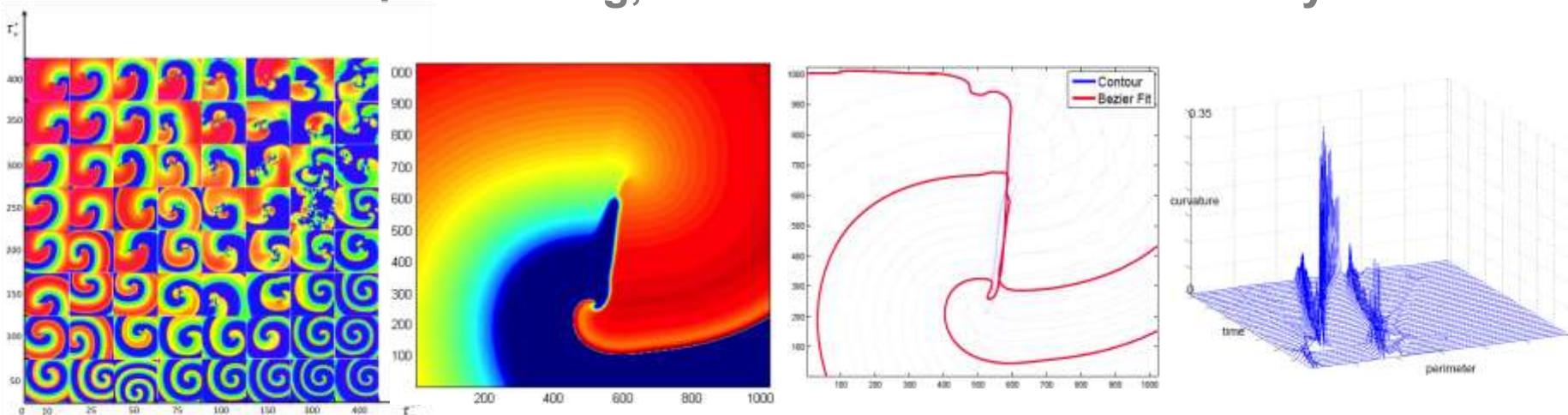
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- Derive the MRM from Iyer model through TS abstraction